

# **Mechanisms of Exertional Dyspnea in Symptomatic Smokers without COPD**

Amany F. Elbehairy, Jordan A. Guenette, Azmy Faisal, Casey E. Ciavaglia, Katherine A. Webb, Dennis Jensen, Andrew H. Ramsook, J. Alberto Neder, Denis E. O'Donnell;  
on behalf of the Canadian Respiratory Research Network.

## **ONLINE DATA SUPPLEMENT**

### **METHODS**

#### **Oxygen Cost Diagram**

The oxygen cost diagram was used to evaluate self-reported tolerance of daily activities. This scale consists of a 100 mm line listing everyday activities in proportion to their approximate oxygen cost between zero and 100. Subjects were asked to indicate the point on the line, beyond which they became breathless. The distance from point zero was measured and reported in mm (E1).

#### **Pulmonary Function Tests**

Detailed pulmonary function tests were performed using automated equipment (Vmax229d and Autobox V62J; and MasterScreen impulse oscillometry (IOS); SensorMedics, Yorba Linda, CA); measurements were expressed relative to predicted normal values (E2-E7).

#### **Anaerobic Threshold Assessment**

The anaerobic threshold (AT) was assessed using the V-slope method (E8,E9). For corroboration of the V-slope method, we also employed the ventilatory equivalent method (E10,E11). Furthermore, two different investigators independently verified the identification of the AT.

#### **Diaphragm Electromyography and Respiratory Pressure Measurements**

Diaphragm electromyography (EMGdi), esophageal pressure (Pes) and gastric pressure (Pga) were measured continuously using a combined electrode-balloon catheter system (E12-E21).

Due to the subjective analysis of the EMGdi analysis, the same investigator examined data for both smokers and healthy controls in a blinded fashion. The EMGdi signal was sampled at 2000 Hz (PowerLab, model ML880; ADInstruments, CastleHill, NSW, Australia), band-pass filtered between 20-1000 Hz (Bioamplifier model RA-8; Guanzhou Yinghui Medical Equipment Co. Ltd, Guangzhou, China) and converted to a root mean square; the largest value from the five electrode pairs in each inspiration was used for analysis. The esophageal and gastric balloons were inflated with 1.0 mL and 1.2 mL of air, respectively. Pes and Pga were measured using differential pressure transducers (model DP15-34; Validyne Engineering, Northridge, CA, USA) and sampled at a rate of 100 Hz (PowerLab); transdiaphragmatic pressure (Pdi) was calculated by electronic subtraction of Pes from Pga. The continuous flow signal from the cardiopulmonary exercise testing system (Vmax229d; SensorMedics, Yorba Linda, CA) was simultaneously input into the data acquisition system for analysis.

Maximal EMGdi (EMGdi,max) was determined during serial inspiratory capacity (IC) maneuvers at rest and throughout exercise (E17,E22); EMGdi,max measured in this way often produces greater values than during sniff maneuvers, and has been shown to be highly reproducible and remains unchanged during ventilatory stimulation by exercise or hypercapnia (E15,E23,E24). EMGdi/EMGdi,max was used as an index of inspiratory neural drive to the crural diaphragm. IC maneuvers at rest and throughout exercise were used to obtain dynamic peak inspiratory Pdi (Pdi,max) (E19,E20). Inspiratory Pdi was the peak tidal value during inspiration; inspiratory Pdi/Pdi,max was used as an index of diaphragmatic effort. Tidal Pes swings were defined as the amplitude between the maximum inspiratory and expiratory values for each respiratory cycle. Tidal Pes swings were expressed as a fraction of the difference between the maximum values during the IC maneuvers and the baseline vital capacity maneuver;

$P_{es}/P_{es,max}$  was used as an index of global respiratory effort. The expiratory rise in  $P_{ga}$  ( $P_{ga,exp.rise}$ ) was used as an index of expiratory muscle activity (E25).

End-inspiratory (EI) and end-expiratory (EE) data points of zero flow for  $P_{es}$  and  $P_{ga}$  were collected. Dynamic compliance ( $C_{L,dyn}$ ) was calculated as the difference in lung volume divided by difference in  $P_{es}$  between EE and EI (E26). Total lung resistance was calculated as the difference in  $P_{es}$  divided by the difference in flow at inspiratory mid-volume and expiratory iso-volume ( $\Delta P_{es}/\Delta flow$ ) (E26). The tension time index of the diaphragm (TTIdi) and the inspiratory muscles (TTIes) was calculated as the product of tidal  $P_{di}$  and  $P_{es}$  and the ratio of inspiration time to breath cycle (E27,E28). The mechanical work of breathing was determined as the area within an ensemble averaged tidal  $P_{es}$ -volume loop with the addition of that portion of a triangle representing work that fell outside of the pressure-volume loop (i.e., part of the elastic work of breathing) (E29) and was further subdivided into the inspiratory resistive and inspiratory elastic work of breathing (E30).

## **RESULTS**

### **Subjects**

Comorbidities within the smokers group included stable: hypertension (n=5), gastro-esophageal reflux disease (n=4), mild liver disease (n=2), previous myocardial infarction (n=1), and diabetes mellitus (n=1). None were treated for congestive heart failure. All smokers did not meet spirometric criteria for COPD, i.e., a post-bronchodilator  $FEV_1/FVC$  was  $> 0.7$  and higher than the predicted lower limit of normal (LLN), except one subject who had a ratio lower than LLN by only 0.5%. In support of successful asthma exclusion, none of the smokers demonstrated significant bronchodilator reversibility.

## Cardiopulmonary Exercise Test

Smokers had a reduced peak work rate and oxygen uptake ( $\dot{V}O_2$ ) compared with controls; however,  $\dot{V}O_2$ -work rate relationships were superimposed in both groups throughout exercise (**Figure E1**). Heart rate and oxygen pulse responses were similar throughout exercise but smokers reached a lower peak heart rate than controls (mean $\pm$ SD): 75 $\pm$ 15 versus 94 $\pm$ 7 %predicted ( $P<0.05$ ) (**Figure E1**). Intensity ratings of leg discomfort during exercise were significantly greater in smokers compared to controls (**Figure E1**).

The ventilatory equivalent for carbon dioxide ( $\dot{V}_E/\dot{V}CO_2$ ) was not different at its nadir during exercise between the two groups (28.7 $\pm$ 3.3 versus 27.9 $\pm$ 3.3; smokers versus controls). However, those (n=10) with values above the median of 28 (n=10) had a significantly lower peak  $\dot{V}O_2$  than those below the median (n=10): 56 $\pm$ 24 versus 101 $\pm$ 41 %predicted, respectively ( $P=0.007$ ). Within smokers, the  $\dot{V}_E/\dot{V}CO_2$  nadir correlated well with peak  $\dot{V}O_2$  ( $R= -0.598$ ,  $P=0.005$ ) (**Figure E2**).

Fourteen subjects in each group accepted the insertion of the EMGdi-pressure catheter. Indices of global inspiratory muscle effort (inspiratory  $P_{es}/P_{i,max}$ ) and expiratory muscle activity ( $P_{ga}$  expiratory rise) were similar between both groups (**Figure E1, E3**). EMGdi relative to maximum (EMGdi/EMGdi,max), inspiratory  $P_{di}/P_{di,max}$  and total lung resistance were significantly ( $P<0.05$ ) higher for a given ventilation ( $\dot{V}_E$ ) in smokers compared with controls (**Figure E3**).

Looking at individual EMGdi data, there were several smokers with tidal EMGdi values at rest and early in exercise that were higher than any seen in the control group. In addition, the majority of smokers had EMGdi,max values during their serial IC maneuvers in the low range (i.e., <100  $\mu$ V) in contrast to the control group where the majority had values in the higher range (i.e., >150  $\mu$ V) (**Figure E4**); EMGdi,max during the highest IC was lower in smokers versus

controls ( $113\pm 65$  versus  $165\pm 56$   $\mu\text{V}$ ,  $P=0.028$ ). Thus, the higher  $\text{EMGdi}/\text{EMGdi,max}$  reflected differences in both the numerator (tidal  $\text{EMGdi}$ ) and the denominator ( $\text{EMGdi,max}$ ) which varied between smokers. Of note,  $\text{EMGdi}/\text{EMGdi,max}$  was significantly higher in smokers at rest and throughout exercise whether  $\text{EMGdi,max}$  was calculated during serial IC maneuvers, the highest IC throughout the test, or the highest inspiratory maneuver (either IC or sniff) throughout the test (**Figure E5**). Values of pre- and post-exercise maximal respiratory pressures and  $\text{EMGdi}$  during sniff and IC maneuvers are summarized in **Table E1**.

## REFERENCES

- E1. McGavin CR, Artvinli M, Naoe H, McHardy GJ. Dyspnoea, disability, and distance walked: comparison of estimates of exercise performance in respiratory disease. *Br Med J* 1978; 2: 241–243.
- E2. Buist AS, Ross BB. Quantitative analysis of the alveolar plateau in the diagnosis of early airway obstruction. *Am Rev Respir Dis* 1973; 108(5): 1078–1087.
- E3. Morris JF, Koski A, Temple WP, Claremont A, Thomas DR. Fifteen year interval spirometric evaluation of the Oregon predictive equations. *Chest* 1988; 93: 123–127.
- E4. Crapo RO, Morris AH, Clayton PD, Nixon CR. Lung volumes in healthy nonsmoking adults. *Bull Eur Physiopathol Respir* 1982; 18: 419–425.
- E5. Burrows B, Kasik JE, Niden AH, Barclay WR. Clinical usefulness of the single-breath pulmonary diffusing capacity test. *Am Rev Respir Dis* 1961; 84: 789–806.
- E6. Briscoe WA, Dubois AB. The relationship between airway resistance, airway conductance and lung volume in subjects of different age and body size. *J Clin Invest* 1958; 37: 1279–1285.
- E7. Hamilton AL, Killian KJ, Summers E, Jones NL. Muscle strength, symptom intensity, and exercise capacity in patients with cardiorespiratory disorders. *Am J Respir Crit Care Med* 1995; 152: 2021–2031.
- E8. Wasserman K. The anaerobic threshold measurement to evaluate exercise performance. *Am Rev Respir Dis* 1984; 129(Suppl): S35–S40.
- E9. Beaver WL, Wasserman K, Whipp BJ. A new method for detecting anaerobic threshold by gas exchange. *J Appl Physiol* 1986; 60(6): 2020–2027.
- E10. Reinhard U, Müller PH, Schmülling RM. Determination of anaerobic threshold by ventilation equivalent in normal individuals. *Respiration* 1979; 38: 36–42.
- E11. Gaskill SE, Ruby BC, Walker AJ, Sanchez OA, Serfass RC, Leon AS. Validity and reliability of combining three methods to determine ventilatory threshold. *Med Sci Sports Exerc* 2001; 33(11): 1841–1848.
- E12. Luo YM, Moxham J. Measurement of neural respiratory drive in patients with COPD. *Respir Physiol Neurobiol* 2005; 146: 165–174.
- E13. Luo YM, Moxham J, Polkey MI. Diaphragm electromyography using an oesophageal catheter: Current concepts. *Clin Sci (Lond)* 2008; 115: 233–244.
- E14. Jolley CJ, Luo YM, Steier J, Reilly C, Seymour J, Lunt A, Ward K, Rafferty GF, Polkey MI, Moxham J. Neural respiratory drive in healthy subjects and in COPD. *Eur Respir J* 2009; 33: 289–297.

- E15. Luo YM, Li RF, Jolley C, Wu HD, Steier J, Moxham J, Zhong NS. Neural respiratory drive in patients with COPD during exercise tests. *Respiration* 2011; 81(4): 294–301.
- E16. Ora J, Laveneziana P, Wadell K, Preston M, Webb KA, O'Donnell DE. Effect of obesity on respiratory mechanics during rest and exercise in COPD. *J Appl Physiol* 2011; 111: 10–19.
- E17. Jensen D, O'Donnell DE, Li R, Luo YM. Effects of dead space loading on neuro-muscular and neuro-ventilatory coupling of the respiratory system during exercise in healthy adults: implications for dyspnea and exercise tolerance. *Respir Physiol Neurobiol* 2011; 179: 219–226.
- E18. Laveneziana P, Webb KA, Wadell K, Neder JA, O'Donnell DE. Does expiratory muscle activity influence dynamic hyperinflation and exertional dyspnea in COPD? *Respir Physiol Neurobiol* 2014; 199: 24–33.
- E19. Guenette JA, Chin RC, Cheng S, Dominelli PB, Raghavan N, Webb KA, Neder JA, O'Donnell DE. Mechanisms of exercise intolerance in Global Initiative for Chronic Obstructive Lung Disease grade 1 COPD. *Eur Respir J* 2014; 44: 1177–1187.
- E20. Ciavaglia CE, Guenette JA, Langer D, Webb KA, Neder JA, O'Donnell DE. Differences in respiratory muscle activity during cycling and walking do not influence dyspnea perception in obese patients with COPD. *J Appl Physiol* 2014; 117(11): 1292–1301.
- E21. Jolley CJ, Luo YM, Steier J, Rafferty GF, Polkey MI, Moxham J. Neural respiratory drive and breathlessness in COPD. *Eur Respir J* 2015; 45(2): 355–364.
- E22. Sinderby C, Beck J, Spahija J, Weinberg J, Grassino A. Voluntary activation of the human diaphragm in health and disease. *J Appl Physiol* 1998; 85: 2146–2158.
- E23. Zhang D, Gong H, Lu G, Guo H, Li R, Zhong N, Polkey MI, Luo Y. Respiratory motor output during an inspiratory capacity maneuver is preserved despite submaximal exercise. *Respir Physiol Neurobiol* 2013; 189: 87–92.
- E24. Singh B, Panizza JA, Finucane KE. Diaphragm electromyogram root mean square response to hypercapnia and its intersubject and day-to-day variation. *J Appl Physiol* 2005; 98: 274–281.
- E25. Yan S, Sinderby C, Bielen P, Beck J, Comtois N, Sliwinski P. Expiratory muscle pressure and breathing mechanics in chronic obstructive pulmonary disease. *Eur Respir J* 2000; 16: 684–690.
- E26. Tobin MJ. Monitoring respiratory mechanics in spontaneously breathing patients. In: Tobin MJ (eds.). *Principles and Practice of Intensive Care Monitoring*. New York: McGraw-Hill; 1997. p. 617–654.
- E27. Petrof BJ, Legaré M, Goldberg P, Milic-Emili J, Gottfried SB. Continuous positive airway pressure reduces work of breathing and dyspnea during weaning from mechanical ventilation in severe chronic obstructive pulmonary disease. *Am Rev Respir Dis* 1990; 141(2): 281–289.

- E28. Maltais F, Reissmann H, Gottfried SB. Pressure support reduces inspiratory effort and dyspnea during exercise in chronic airflow obstruction. *Am J Respir Crit Care Med* 1995; 151(4): 1027–1033.
- E29. McGregor M, Becklake MR. The relationship of oxygen cost of breathing to respiratory mechanical work and respiratory force. *J Clin Invest* 1961; 40: 971–980.
- E30. Dominelli PB, Sheel AW. Experimental approaches to the study of the mechanics of breathing during exercise. *Respir Physiol Neurobiol* 2012; 180: 147–161.



**TABLE E1.** Pre- and post-exercise maximal respiratory pressures and EMGdi during sniff and IC maneuvers

Variable	Smokers without COPD		Healthy Controls	
	Pre-exercise	Post-exercise	Pre-exercise	Post-exercise
Pes,sniff, cmH <sub>2</sub> O	69 ± 14	71 ± 14	70 ± 13	69 ± 16
Pes,IC, cmH <sub>2</sub> O	39 ± 10	42 ± 10	41 ± 11	41 ± 10
Pdi,sniff, cmH <sub>2</sub> O	96 ± 23	89 ± 22†	108 ± 17	95 ± 24†
Pdi,IC, cmH <sub>2</sub> O	64 ± 19	57 ± 17†	76 ± 23	60 ± 20†
EMGdi,sniff, μV	117 ± 51*	116 ± 58*	159 ± 66	150 ± 50
EMGdi,IC, μV	98 ± 55*	101 ± 64*	150 ± 47	153 ± 48

Values are means ± SD.

\* $P < 0.05$  smokers without COPD versus healthy controls. † $P < 0.05$  pre- versus post-exercise within each group.

*Abbreviations:* IC = inspiratory capacity; EMGdi = diaphragm electromyography; Pes = esophageal pressure; Pdi = transdiaphragmatic pressure.

## FIGURES LEGENDS

**Figure E1.** Intensity ratings of leg discomfort (**a**) oxygen uptake (**b**), heart rate (**c**), oxygen pulse (**d**),  $P_{es}/P_{i,max}$  (**e**),  $P_{ga}$  expiratory rise (**f**) are plotted against work rate during incremental cycle exercise in smokers without COPD and in age-matched healthy controls. Values are mean $\pm$ SEM. \* $P < 0.05$  smokers without COPD vs. healthy controls at standardized work rates or at peak exercise. *Abbreviations:*  $VO_2$  = oxygen uptake;  $P_{es}$  = esophageal pressure;  $P_{es}/P_{i,max}$  = inspiratory esophageal pressure relative to maximum and used as an index of global inspiratory muscle effort;  $P_{ga}$  = gastric pressure;  $P_{ga}$  expiratory rise = an index of expiratory muscle activity.

**Figure E2.** There was a significant inverse relationship between the ventilatory equivalent for carbon dioxide ( $V_E/V_{CO_2}$ ) at its nadir and peak  $VO_2$  during exercise in smokers without COPD ( $R = -0.598$ ,  $P = 0.005$ ).

**Figure E3.** Diaphragm electromyography (EMG<sub>di</sub>) and select pressure-derived respiratory mechanical measurements are shown during incremental cycle exercise in smokers without COPD and age-matched healthy controls. Values are mean $\pm$ SEM. \* $P < 0.05$  smokers without COPD vs. healthy controls at a standardized ventilation or at peak exercise. *Abbreviations:* EMG<sub>di</sub>/EMG<sub>di,max</sub> = EMG<sub>di</sub> relative to maximum is an indirect measure of inspiratory neural drive to the crural diaphragm; tidal  $P_{es}/P_{es,max}$  = tidal esophageal pressure relative to maximum is an index of total respiratory muscle effort; tension time index,  $t_{es}$  = tension time index derived from esophageal pressure is an index of the oxygen cost of breathing; inspiratory  $P_{di}/P_{di,max}$  = inspiratory transdiaphragmatic pressure relative to maximum is an index of diaphragmatic effort;  $P_{ga}$  = gastric pressure; WOB = work of breathing.

**Figure E4.** Individual diaphragm electromyography (EMGdi) data are shown during incremental cycle exercise in smokers without COPD and age-matched healthy controls. Data are shown as absolute tidal inspiratory EMGdi (*panels a and c*) and as maximum values during serial IC maneuvers (*panels b and d*) at rest and during exercise in both smokers and healthy controls. *Abbreviations:* IC = inspiratory capacity; insp = inspiratory.

**Figure E5.** Diaphragm electromyography (EMGdi) relative to maximum (EMGdi,max) is shown during incremental cycle exercise in smokers without COPD and age-matched healthy controls. EMGdi,max was derived during concurrent serial inspiratory capacity (IC) maneuvers (*panel a*), during the highest IC maneuver throughout the test (*panel b*), or during the highest inspiratory maneuver (either IC or sniff) throughout the test (*panel c*). Values are mean±SEM. \* $P < 0.05$  smokers without COPD vs. healthy controls at rest or at a standardized work rates.