## APPENDIX D:

## **Calculation of Delivered Dose**

## Example of an alternate delivery system

Recent work[1] has been conducted to evaluate dose delivery from nebulizer systems having higher output than the English Wright. In vitro data suggest that tidal breathing from one high efficiency device, driven by a 50 psi dry gas source, would result in pulmonary deposition equivalent to two minutes from the English Wright in approximately 12 seconds. Because of concern that 12 seconds could lead to too much variability in the number of breaths, a comparative *in vivo* study done in children[2] was carried out using a 20 second time period. Data from that study showed that the  $PC_{20}$  was approximately one doubling concentrations less for the high output delivery system compared to two minutes of tidal breathing with the English Wright. A recent study has confirmed these results in adults[3]. However, when the cumulative *dose* of methacholine required to cause a 20% fall in FEV<sub>1</sub>, the PD<sub>20</sub>, was calculated[2], the results using the two devices were virtually identical. In a reanalysis of this data, the PD<sub>20</sub> results calculated from the non-cumulative final step doses for the two devices were also virtually identical[4]. The step doses were the expected pulmonary dose delivered, based on the nebulizer performance in vitro, a Ti/Ttot ratio of 0.4 and the duration of breathing[1]. This demonstrates a major advantage of using the PD<sub>20</sub> as compared to the PC<sub>20</sub>; that is, if the performance characteristics of the delivery systems are known, there should be little difference in the PD<sub>20</sub> calculated from one device or protocol compared to another. This is clearly not the case for the PC<sub>20</sub>, which may give rise to error and confusion when devices or protocols other than those for which reference data exist are used. An example of calculating the dose steps based on device output is shown below.

For two minutes of tidal breathing from the English Wright:

With a 16 mg/mL solution, a filter at the "mouth" of a breath simulator collected 0.19 mg/min, all of which was carried in droplets < 5  $\mu$ m so would be expected to deposit in the lungs if inhaled (a Respirable Fraction of 1). Hence, for 2 min breathing, the delivered dose would be:

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0.19 mg/mL x 1 x 2 = 0.38 mg (380 \mug) and for other dilutions:

Dose = [conc(mg/mL)/16 mg/mL] x 380 \mug.
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For 20 seconds of tidal breathing from the high output device:

With a 16 mg/mL solution, the rate of a filter collection at the "mouth" was 2.70 mg/min with 76% in droplets < 5  $\mu$ m. Hence for 20 seconds breathing 16 mg/mL, the delivered dose would be:

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2.70 mg/min \times 0.76 \times 20/60 min = 0.68 mg (680 \mug) and for other dilutions:
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Dose =  $[conc(mg/mL)/16 mg/mL] \times 680 \mu g$ .

If the only data available is the continuous output of the nebulizer carried in in droplets < 5  $\mu$ m, the output should be multiplied by a Ti/Ttot ratio of 0.4 to give the expected rate of pulmonary deposition during tidal breathing.

The same principles of dose calculation would apply to a dosimeter driven delivery system. If a dosimeter is used with tidal or submaximal inspirations, then the calculation requires output per actuation, fraction of the aerosol carried in droplets  $\leq$  5 µm and breath number.

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