



# Intrapulmonary shunt and alveolar dead space in a cohort of patients with acute COVID-19 pneumonitis and early recovery

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**Hypoxaemia in COVID-19 is due to a variable combination of intrapulmonary shunt and increased dead space, likely from both airspace and vascular pathology. Increased dead space present up to 2 months later suggests persistent pulmonary vascular pathology.** <https://bit.ly/3ROTboc>

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## Abstract

**Background** Pathological evidence suggests that coronavirus disease 2019 (COVID-19) pulmonary infection involves both alveolar damage (causing shunt) and diffuse microvascular thrombus formation (causing alveolar dead space). We propose that measuring respiratory gas exchange enables detection and quantification of these abnormalities. We aimed to measure shunt and alveolar dead space in moderate COVID-19 during acute illness and recovery.

**Methods** We studied 30 patients (22 males; mean±SD age 49.9±13.5 years) 3–15 days from symptom onset and again during recovery, 55±10 days later (n=17). Arterial blood (breathing ambient air) was collected while exhaled oxygen and carbon dioxide concentrations were measured, yielding alveolar–arterial differences for each gas ( $P_{A-aO_2}$  and  $P_{a-ACO_2}$ , respectively) from which shunt and alveolar dead space were computed.

**Results** For acute COVID-19 patients, group mean (range) for  $P_{A-aO_2}$  was 41.4 (–3.5–69.3) mmHg and for  $P_{a-ACO_2}$  was 6.0 (–2.3–13.4) mmHg. Both shunt (% cardiac output) at 10.4% (0–22.0%) and alveolar dead space (% tidal volume) at 14.9% (0–32.3%) were elevated (normal: <5% and <10%, respectively), but not correlated ( $p=0.27$ ). At recovery, shunt was 2.4% (0–6.1%) and alveolar dead space was 8.5% (0–22.4%) (both  $p<0.05$  versus acute). Shunt was marginally elevated for two patients; however, five patients (30%) had elevated alveolar dead space.

**Conclusions** We speculate impaired pulmonary gas exchange in early COVID-19 pneumonitis arises from two concurrent, independent and variable processes (alveolar filling and pulmonary vascular obstruction). For most patients these resolve within weeks; however, high alveolar dead space in ~30% of recovered patients suggests persistent pulmonary vascular pathology.

## Introduction

Since the beginning of 2020, over half a billion people have been diagnosed with coronavirus disease 2019 (COVID-19), a disease caused by infection with the novel severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2). Many have required hospitalisation, with 10–20% of those requiring intensive care, mainly due to respiratory compromise [1]. Worldwide there have been more than 6 million deaths.

Patients with early COVID-19 respiratory failure present with hypoxaemia and hyperventilation [2–6]. The hypoxaemia is likely related to ventilation/perfusion ( $V_A/Q'$ ) mismatch and in particular to increased intrapulmonary shunt arising from alveolar filling with fluid or cellular debris. However, pathology reports from COVID-19 infected lungs also frequently demonstrate pulmonary vasculature involvement, including



severe endothelial injury, widespread thrombosis with microangiopathy and new vessel growth [7–9]. Pulmonary vessel microembolism reduces capillary blood flow, thus generating areas of high  $V'_A/Q'$  and promoting increased alveolar dead space.

We hypothesised that in early COVID-19 pneumonitis, hypoxaemia is associated with both increased intrapulmonary shunt and increased alveolar dead space. Using bedside measurement of exhaled partial pressure of oxygen ( $P_{O_2}$ ) and carbon dioxide ( $P_{CO_2}$ ) combined with arterial blood gas measurements, we measured alveolar–arterial partial pressure differences for both oxygen ( $P_{A-aO_2}$ ) and carbon dioxide ( $P_{A-aCO_2}$ ), from which both intrapulmonary shunt and alveolar dead space values were then determined using a novel computational model [10].

## Methods

### Subjects

30 patients admitted to Danderyd Hospital in Stockholm, Sweden who were  $\geq 18$  years old and PCR-positive for SARS-CoV-2 were recruited between November and December 2020. Patients were excluded if they were in immediate need of intubation or mechanical ventilation, had advanced pulmonary or cardiac disease, current malignancy, previous thromboembolic disease, current pregnancy, or were unable to tolerate the study protocol, which required spontaneous breathing of ambient air for several minutes. Data were collected within 24 h of presentation to hospital and again  $55 \pm 10$  days after discharge in early recovery ( $n=17$ ). 13 patients did not return for follow-up. A subset of the acute data has been reported previously [6].

13 healthy volunteers, negative for SARS-CoV-2 on PCR testing and with normal pulmonary function (Vyair-Vyntus Spiro PC-spirometer with SentrySuite Software; Vyair, Mettawa, IL, USA), were recruited from hospital staff as methodological controls.

All participants gave written informed consent and the study protocol was approved by the Swedish Ethical Review Authority (diary number 2020-02966).

### Clinical data

Anthropometric and demographic data were collected, along with body temperature for the acutely ill. Pathology test results, pharmacological interventions, respiratory support (including oxygen therapy) and duration of hospitalisation data were also collected.

### Study protocol

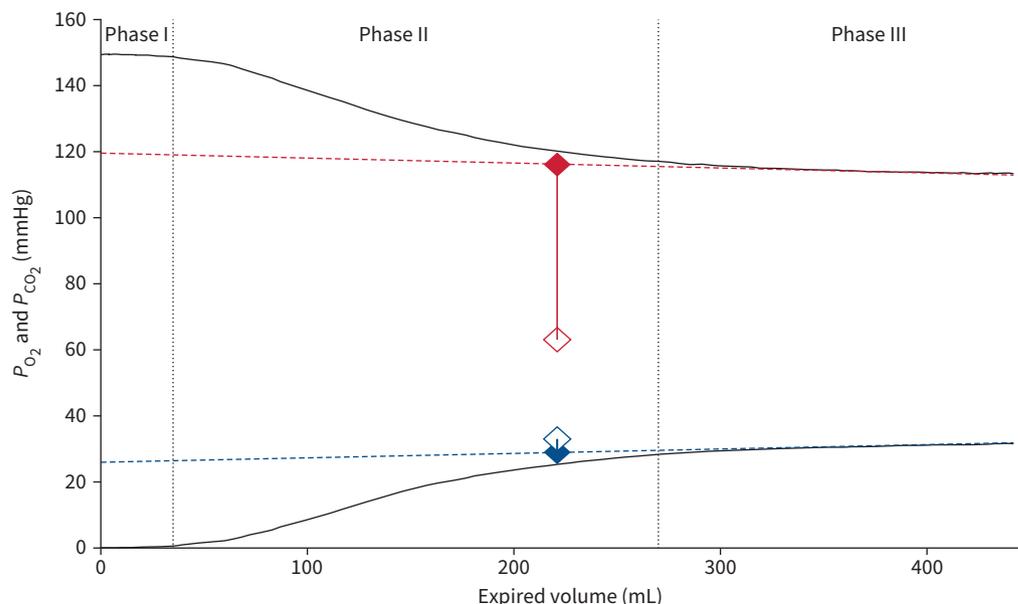
Subjects were studied in a semirecumbent position, wearing a noseclip and breathing ambient air *via* a mouthpiece with an antivirus filter (MicroGard II; Vyair Medical, Hoechst, Germany; apparatus dead space 75 mL) attached to an inspired/expired gas measurement system (Oxycon Pro; Vyair Medical). Collected data included  $P_{O_2}$ ,  $P_{CO_2}$  and respiratory gas flow at high sampling frequency (100 Hz). After a few minutes of adaptation, participants maintained steady-state breathing (end-tidal  $P_{CO_2}$  within  $\pm 2$  mmHg across several breaths) at a (metronome-facilitated) frequency and tidal volume of their choice. Data were recorded over a steady-state 3–5 min period, during which radial arterial blood was collected over several breaths and then processed immediately (ABL800 Flex Plus; Radiometer Medical, Bronshøj, Denmark) to obtain values for arterial  $P_{O_2}$  ( $P_{aO_2}$ ) and  $P_{CO_2}$  ( $P_{aCO_2}$ ). For the acute patient studies, arterial blood gas values were expressed at body temperature [11]. Recovered patients and healthy subjects were assumed to have a body temperature of 37°C.

### Exhaled gas analysis

Three separate breaths, preceding the arterial blood sample by  $35 \pm 10$  s, were selected, independently analysed and resulting parameters averaged. Following alignment of gas and volume signals,  $P_{O_2}$  and  $P_{CO_2}$  values for each breath were plotted as a function of expired volume and a linear least-squares fit applied to the alveolar plateau (phase III; see figure 1). Mean alveolar gas values,  $P_{AO_2}$  and  $P_{ACO_2}$  [10], at the mid-point (by volume) of the expired breath were determined from the fitted lines. Exhaled gas measurements in the acute patient studies were corrected for water vapour pressure at body temperature using Antoine's formula [12]. Alveolar–arterial partial pressure differences for both  $O_2$  and  $CO_2$  were then calculated as  $P_{AO_2} - P_{aO_2}$  ( $P_{A-aO_2}$ ) and  $P_{aCO_2} - P_{ACO_2}$  ( $P_{a-ACO_2}$ ).

### Computational analysis

We employed the seven-decade-old RILEY and COURNAND [13] three-compartment lung model to calculate shunt and alveolar dead space from  $P_{A-aO_2}$  and  $P_{a-ACO_2}$ . In this model, the lung is considered to have an intrapulmonary shunt compartment with a  $V'_A/Q'$  of zero, also encompassing regions of very low  $V'_A/Q'$ ,



**FIGURE 1** Expired gas tracings from one patient: exhaled partial pressure of oxygen ( $P_{O_2}$ ; top black line, red symbols and lines) and carbon dioxide ( $P_{CO_2}$ ; bottom black line, blue symbols and lines). The second dotted line indicates the beginning of alveolar emptying (phase III), sloping dashed lines indicate the linear regression fits to phase III. Alveolar partial pressures ( $P_{ACO_2}$  and  $P_{AO_2}$ ) were measured from the mid-volume of the linear regression fit to phase III (~225 mL in this example). Filled symbols indicate mean alveolar values; open symbols indicate contemporaneous arterial values; arterial-alveolar differences are indicated by the solid vertical lines connecting the symbols.

and an alveolar dead space compartment with  $V'_A/Q'$  of infinity, also encompassing regions of very high  $V'_A/Q'$ . The remainder of the lung is assumed to be normal, with a  $V'_A/Q'$  ratio given by non-dead space ventilation divided by non-shunt blood flow. A critical difference exists between the Riley and Courmand model and the current approach: Riley and Courmand used the venous admixture equation for oxygen to calculate shunt and the Bohr equation for carbon dioxide to calculate dead space. However, shunt may increase arterial  $P_{CO_2}$  and contribute to calculated alveolar dead space, while dead space (without compensatory hyperventilation) lowers arterial  $P_{O_2}$  and contributes to calculated shunt. Our approach [10] recognises this complexity and resolves it, still within the three-compartment framework, by determining the values of shunt and dead space that, present together, predict the measured arterial and expired alveolar  $P_{O_2}$  and  $P_{CO_2}$  values, and hence their partial pressure differences. In addition, the Bohr equation usually includes anatomical dead space, which commonly dominates total dead space numbers. Our approach eliminates anatomical dead space by using mean alveolar partial pressures as in figure 1 and not those of mixed exhaled gas.

Using the measured  $V'_{CO_2}$  (respiratory frequency  $\times$  volume  $CO_2$  per breath),  $P_{AO_2}$ , fractional alveolar oxygen concentration ( $F_{AO_2}$ ),  $P_{ACO_2}$  and fractional alveolar carbon dioxide concentration ( $F_{ACO_2}$ ), we calculated: 1) total expired alveolar ventilation  $V'_A = V'_{CO_2}/F_{ACO_2}$ , 2) inspired alveolar ventilation  $V'_I = V'_A \times ((1 - F_{AO_2}) - F_{ACO_2}) / (1 - F_{IO_2})$  and 3)  $V'_{O_2} = V'_I \times F_{IO_2} - V'_A \times F_{AO_2}$ , where  $F_{IO_2}$  is the inspiratory oxygen fraction.

Cardiac output ( $Q'_T$ ) was then estimated as  $Q'_T = V'_{O_2} + 5$ , with both  $Q'_T$  and  $V'_{O_2}$  expressed in  $L \cdot \text{min}^{-1}$  [14, 15]. The oxygen tension at which haemoglobin is 50% saturated ( $HbP_{50}$ ) was assumed to be 26.8 mmHg. Using these values and each patient's own data for  $V'_{O_2}$ ,  $V'_{CO_2}$ ,  $V'_A$ ,  $Q'_T$ , base excess, haemoglobin concentration and body temperature, we applied the algorithm first published in 1969 by WEST [16] to estimate the values of intrapulmonary shunt and alveolar dead space that would result in the measured  $P_{aO_2}$  and  $P_{aCO_2}$  in each individual to within 0.2 mmHg.

Intrapulmonary shunt was expressed as the percentage of pulmonary blood flow perfusing unventilated regions (shunt %), while alveolar dead space was expressed as the percentage of alveolar ventilation associated with unperfused regions (alveolar dead space %). Based on published measurements using the

**TABLE 1** Anthropometric, demographic and body temperature data for acutely ill COVID-19 patients, recovered COVID-19 patients and healthy subjects

	Acute (n=30)	Recovered (n=17)	Healthy (n=13)
Age (years)	49.9±13.5 (23–78)	50.6±12.0 (51–78)	51.1±17.0 (34–68)
Sex			
Female	8	6	5
Male	22	11	8
Weight (kg)	87.5±17.0 (46–113)	87.5±18.2 (46–110)	80.2±26.1 (58–110)
Height (cm)	177.0±11.3 (150–195)	176.8±13.2 (150–195)	177.2±19.5 (159–198)
BMI (kg·m <sup>-2</sup> )	27.8±4.3 (20.2–38.5)	27.9±4.7 (20.4–38.5)	25.5±6.0 (19.6–31.5)
Body temperature (°C)	38.0±1.0 (36.5–40.0)	37.0 <sup>#</sup>	37.0 <sup>#</sup>

Data are presented as mean±sd (range) or n. #: assumed.

multiple inert gas elimination technique in normal subjects [17], the 95% upper confidence limit for physiological shunt is 5% and for alveolar dead space is 10%. Further methodological details can be found elsewhere [10].

### Statistical analysis

This was an observational study and a sample size was not calculated. Individual data were pooled and reported as group mean with standard deviation or interquartile range. Comparisons were made using paired t-tests. Relationships between variables were examined using Spearman's rank correlation coefficients.  $p < 0.05$  was considered significant.

## Results

### Subject characteristics

See table 1.

### Acute COVID-19 patient data

All patients had moderate disease and were studied at hospital presentation and within 3–15 days of symptom onset. 24 were admitted (mean  $4.0 \pm 2.8$  days, range 1–12 days); of these, 18 required supplemental oxygen and one was subsequently admitted to the intensive care unit. There were no deaths.

### Pharmacological interventions

22 patients received prophylactic low-molecular-weight heparin (LMWH), 12 of these patients <24 h before the study (tinzaparin 4500 U per day, subcutaneously), while therapeutic LMWH (tinzaparin  $175 \text{ U} \cdot \text{kg}^{-1}$  twice daily, daily, s.c.) was administered to one patient. Post-study, 14 patients received corticosteroids (betamethasone 6 mg orally), three received remdesivir and convalescent plasma was administered to two patients.

### Pathology findings

C-reactive protein levels were elevated in all patients, while almost 40% had elevated levels for D-dimer (table 2).

### Arterial blood gas, oxyhaemoglobin saturation and exhaled alveolar gas data

Arterial blood gas data reflected an acute respiratory alkalosis with hypoxaemia (table 3).  $P_{\text{AO}_2}$  values were all >102 mmHg,  $P_{\text{ACO}_2}$  values were all <38 mmHg and arterial oxygen saturation ( $S_{\text{aO}_2}$ ) values were all >89%.

**TABLE 2** Pathology data at the time of acute COVID-19 infection

Pathology	Mean±sd	Range	Normal range	Abnormal (n (%))
Haemoglobin (g·L <sup>-1</sup> ) (n=29)	139.5±11.7	110–165	Female: 117–153; male: 134–170	2 (6.8)
D-dimer (mg·L <sup>-1</sup> ) (n=28)	0.8±0.6	0.3–3.2	Female: <0.54; male: <0.50	11 (39.2)
C-reactive protein (mg·L <sup>-1</sup> ) (n=30)	79.1±65.7	3–256	<3	30 (100)

TABLE 3 Arterial blood gases and exhaled alveolar gas measurements

	Acute (n=30) <sup>#</sup>	Recovered (n=17)	Healthy (n=13)
pH	7.48±0.04 (7.42–7.60)	7.44±0.03 (7.39–7.51)	7.43±0.02 (7.41–7.49)
$P_{aCO_2}$ (mmHg)	34.8±4.2 (26.5–43.0)	34.4±3.7 (26.7–40.6)	37.0±2.8 (31.4–40.8)
$P_{aO_2}$ (mmHg)	68.3±12.6 (52.3–105.8)	100.6±13.6 (84.0–131.3)	105.0±8.3 (94.5–120.0)
$P_{AO_2}$ (mmHg)	113.3±5.7 (102.2–122.3)	113.6±6.3 (100.2–125.3)	119.5±5.1 (112.7–127.3)
$P_{ACO_2}$ (mmHg)	30.3±4.0 (23.4–37.3)	31.4±3.1 (24.9–38.7)	35.2±2.9 (29.1–39.9)
$P_{A-aO_2}$ (mmHg)	41.4±16.3 (–3.5–69.3)	13.0±9.7 (–6.0–30.2)	6.5±6.9 (–5.8–21.4)
$P_{a-ACO_2}$ (mmHg)	6.0±4.2 (–2.3–13.4)	3.0±2.3 (–2.2–8.9)	1.8±1.9 (–1.4–6.0)
$S_{aO_2}$ (%)	94.3±0.2 (89.4–98.7)	98.7±0.5 (97.7–99.5)	98.9±0.2 (98.4–99.3)

Data are presented as mean±SD (range). <sup>#</sup>: all acute patient gas partial pressures are expressed at body temperature.  $P_{aCO_2}$ : arterial partial pressure of carbon dioxide;  $P_{aO_2}$ : arterial partial pressure of oxygen;  $P_{AO_2}$ : alveolar partial pressure of oxygen;  $P_{ACO_2}$ : alveolar partial pressure of carbon dioxide;  $P_{A-aO_2}$ : alveolar–arterial partial pressure difference for oxygen;  $P_{a-ACO_2}$ : alveolar–arterial partial pressure difference for carbon dioxide;  $S_{aO_2}$ : arterial oxygen saturation.

#### Alveolar–arterial differences

There was wide interpatient variance in  $P_{A-aO_2}$  and  $P_{a-ACO_2}$  (table 3 and figure 2a). Any negative values (expected from experimental noise) were considered to be zero when calculating shunt and dead space.

#### Intrapulmonary shunt and alveolar dead space

Values for intrapulmonary shunt and alveolar dead space varied considerably between patients (table 4 and figure 2b); however, importantly, there was no significant correlation between the shunt and dead space values ( $p=0.27$ ). Significant positive correlations were detected between shunt and both D-dimer ( $r=0.36$ ,  $p=0.03$ ) and CRP ( $r=0.42$ ,  $p=0.01$ ), but not for alveolar dead space ( $p>0.15$ ).

Overall, 23 patients had elevated shunt (defined as  $>5\%$ ), while 22 patients had elevated alveolar dead space (defined as  $>10\%$ ). Simultaneously increased shunt and dead space were present in 19 patients, four patients had elevated shunt but normal alveolar dead space and three had elevated alveolar dead space but normal shunt (figure 2b).

#### Healthy subject data

Healthy subjects were all normoxaemic with normal acid–base status (see table 3). No healthy subject had a shunt value  $>5\%$  (table 4 and figure 2b); two had slightly elevated values for dead space (table 4 and

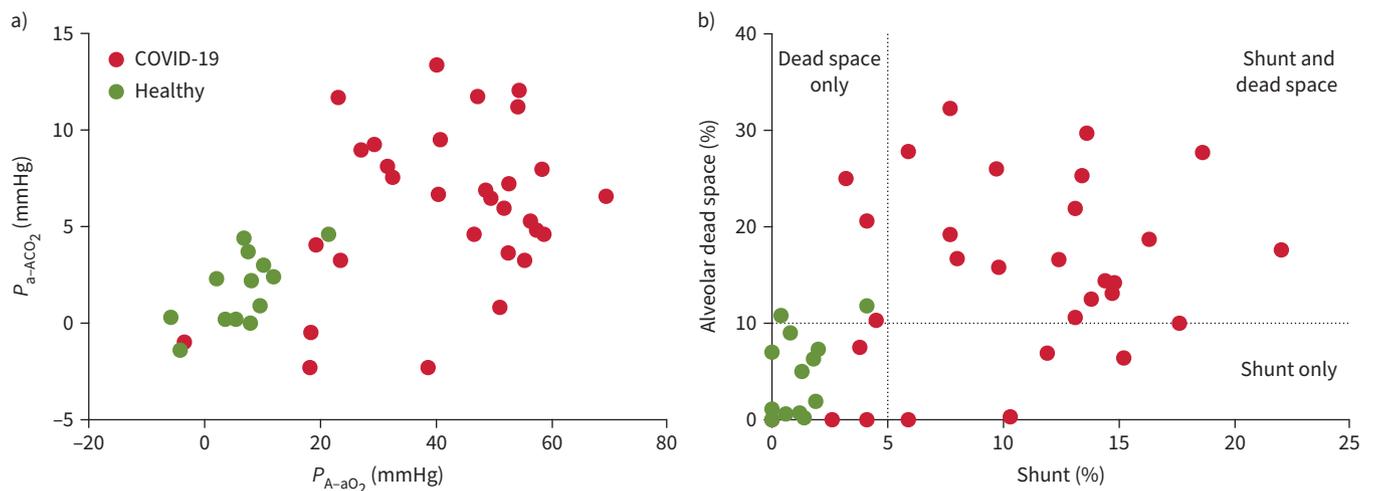


FIGURE 2 a) Alveolar–arterial partial pressure differences for oxygen ( $P_{A-aO_2}$ ) and carbon dioxide ( $P_{a-ACO_2}$ ). b) Intrapulmonary shunt and alveolar dead space. Acute COVID-19 patients (n=30) and healthy subjects (n=13). Dotted lines in (b) show 95% upper limits for normal [17].

**TABLE 4** Shunt and alveolar dead space in acute COVID-19 patients (including the subgroup of 17 patients studied later in recovery), recovered patients and healthy subjects.

	Acute (n=30)	Acute <sup>#</sup> (n=17)	Recovered (n=17)	Healthy (n=13)
Shunt (%)	10.4±5.4 (0–22.0)	11.7±5.1 (4.1–22.0)	2.4±1.9** (0–6.1)	1.2±1.1 (0–4.1)
Alveolar dead space (%)	14.9±9.6 (0–32.3)	14.4±9.7 (0–29.7)	8.6±5.5* (0–22.4)	4.7±4.3 (0–11.8)

Data are presented as mean±SD (range). <sup>#</sup>: subgroup studied in recovery. \*: p<0.05; \*\*: p<0.0001 (compared with acute subgroup).

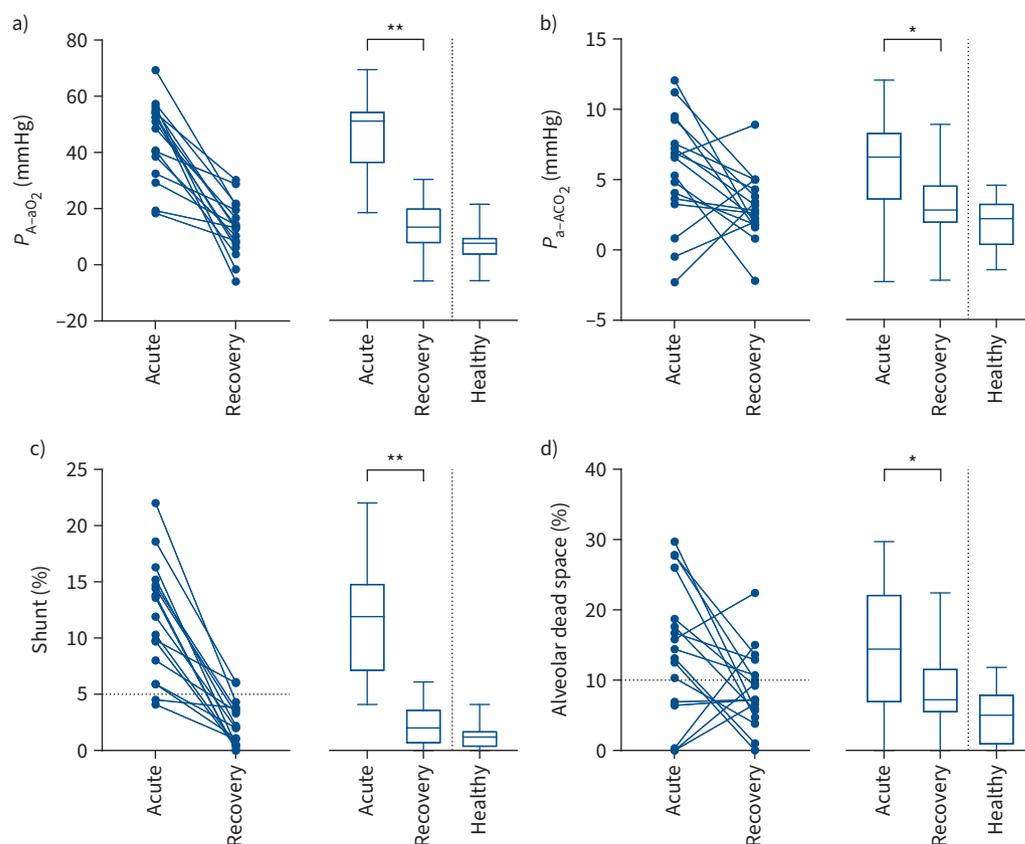
figure 2b). Overall, shunt and dead space values from the healthy subjects conformed to the previously established upper limits of normal [17].

**Transition from acute illness to recovery**

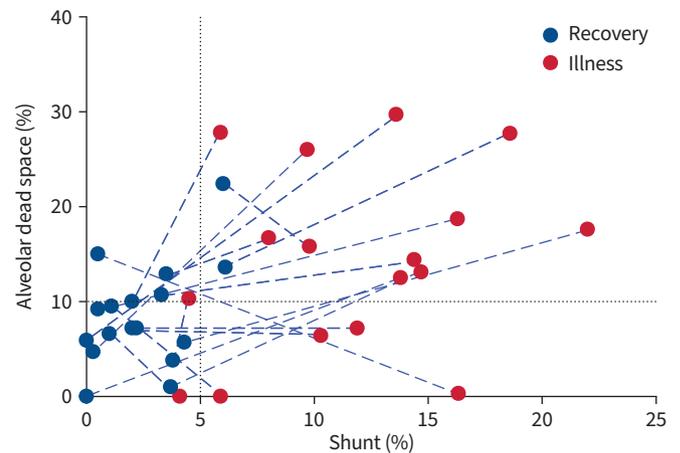
Shunt and alveolar dead space fell significantly following recovery (figures 3 and 4). However, shunt was slightly elevated in two patients, while five patients (29.4%) had elevated dead space. There was no correlation with duration after recovery (both p>0.15).

**Discussion**

Using simultaneous measurements of arterial and exhaled oxygen and carbon dioxide tensions, interpreted using a three-compartment computational lung model, we developed a bedside methodology for quantifying if there is both intrapulmonary shunt and alveolar dead space [10], and then applied it here in



**FIGURE 3** Individual (symbols and lines) and grouped data (box-and-whisker plots showing mean, interquartile range and range) for 17 patients during acute COVID-19 infection and again in early recovery, together with 13 healthy individuals: alveolar–arterial partial pressure differences for a) oxygen ( $P_{A-aO_2}$ ) and b) carbon dioxide ( $P_{A-aCO_2}$ ), and c) shunt and d) alveolar dead space. Horizontal dotted lines in (c) and (d) show the 95% upper confidence intervals for normal. \*: p<0.05; \*\*: p<0.0001.



**FIGURE 4** Shunt and dead space trajectories from acute COVID-19 illness to recovery. Blue dashed lines connect paired acute and recovery data (n=17). Black dotted lines show the 95% upper confidence limits of normal.

the highly infectious disease setting of COVID-19 pneumonitis. Measurements in a healthy subject cohort (technical controls) conformed to historical normal limits previously established by more sophisticated techniques [17].

#### *Pulmonary gas exchange in early COVID-19 pneumonitis*

The main finding from the present study is that in early acute COVID-19 pneumonitis intrapulmonary shunt is elevated for most patients; however, many also have elevated alveolar dead space. Furthermore, intrapulmonary shunt and dead space values were not correlated in moderate COVID-19 pneumonitis. Hence, dead space cannot be predicted from the magnitude of shunt and *vice versa*. This suggests that in early SARS-CoV-2 pulmonary infection two pathophysiologically distinct processes, either separately or together, are in play: 1) patchy alveolar filling/oedema/atelectasis (pneumonia) resulting in lung regions with low or zero  $V_A/Q'$  (*i.e.* shunt) and 2) patchy pulmonary vascular occlusion (emboli) resulting in high  $V_A/Q'$  regions (*i.e.* alveolar dead space). However, the relative contribution of these two processes is highly variable from patient to patient. This is similar to findings in intubated patients with severe acute respiratory distress syndrome, where hypoxaemia is due to increased intrapulmonary shunt and increased dead space [18]. This is the first time that this has been demonstrated physiologically in mild/moderate COVID pneumonitis.

While intrapulmonary shunt is perhaps an expected contributor to hypoxaemia in a pulmonary viral infection [18], previous authors have suggested that for COVID-19 patients shunt values can be so elevated as to be considered “excessive” for the degree of lung injury present [2]. This observation has led to the suggestion that SARS-CoV-2 may specifically impair hypoxic pulmonary vasoconstriction, thus preventing hypoxic pulmonary vasoconstriction-driven restriction of pulmonary capillary blood flow to lung regions with poor or no ventilation, increasing shunt [2, 19]. Whether intrapulmonary shunt values detected in the present study are “excessive” remains undetermined.

A major feature of our results was the high dead space values occurring in 73% of patients, with 63% having both elevated intrapulmonary shunt and dead space and 10% having elevated dead space with no evidence of shunt. Increased alveolar dead space is a consequence of ventilation of underperfused alveoli, and we speculate is consistent with reported diffuse and widespread small pulmonary arterial obstruction from thrombus formation, as detected in pulmonary pathological specimens from deceased COVID-19 patients [7, 20]. This interpretation is further supported by the absence of large vessel emboli on contrast computed tomography imaging (performed for clinical purposes) in a subgroup (n=18) of the present patient cohort, although there was no correlation between dead space and D-dimer.

There is extensive pathological evidence of pulmonary microvascular involvement in COVID-19 pneumonia [20]. Histopathology of patients who died from COVID-19, compared with those who died from influenza, showed microvascular changes present in COVID-19 infected lungs that were not present

with influenza, including endothelial injury, alveolar capillary microthrombi and new vessel growth [7]. In a study which correlated radiological findings with histopathological inflammation in eight patients who died of COVID-19, there was evidence of vascular damage and thrombosis in regions without concurrent airspace involvement [21]. It has been proposed that the vascular injury may precede the development of frank pneumonia and alveolar filling [22].

High  $V'_A/Q'$  regions (dead space) may also be a consequence of redistribution of ventilation from unventilated alveoli (shunt) resulting in relative overventilation of normally perfused alveoli. Our analysis adjusts for any effect of intrapulmonary shunt on  $P_{a-ACO_2}$ , so that redistribution of ventilation from obstructed ventilation zones is unlikely to contribute significantly to our measured dead space values.

#### *Pulmonary gas exchange in early recovery from COVID-19 pneumonitis*

In recovery, intrapulmonary shunt decreased in all patients and values were within normal expected limits for all but two patients (figures 3 and 4). Consequently, ventilation was restored to lung zones previously identified as having no or very low alveolar ventilation. Dead space also decreased in most patients to within, or close to, normal expected limits (figures 3 and 4). However, in five patients, dead space was >10%, ranging from 10.7% to 22.4%. Consequently, for most patients perfusion was restored to lung zones previously identified as having no or very low perfusion. However, for ~30% of those studied in recovery (figures 3d and 4), persistent, or even increasing, dead space values suggest persistent or evolving damage to the pulmonary vasculature. This may be a consequence of pre-morbid disease (e.g. COPD or interstitial lung disease). However, if a consequence of COVID-19 infection, this finding is of particular interest, since recently published data suggest that COVID-19 infection poses increased risk for deep vein thrombosis, pulmonary embolism and bleeding episodes, at 3, 6 and 2 months, respectively, after an acute infection [23].

#### *Clinical implications*

The finding that there is likely both acute and chronic pulmonary microvascular disease in COVID-19 pneumonitis has implications for the clinical management of patients, both in the acute and recovery phases of the disease process. For example, anticoagulation with LMWH has had mixed outcomes, with benefit in moderate disease but no real improvement found in severe disease [24, 25]. Perhaps a clearer picture might emerge if outcomes were stratified by presence or absence of high  $V'_A/Q'$  regions. Targeted therapeutic approaches may then be deployed for patients with increased dead space, who may need anticoagulation, *versus* those with shunt but low dead space, where anticoagulants may, in theory, have risk without major benefits. Application of this methodology could be used in patients with persistent COVID-19 symptoms to better delineate pulmonary pathology.

#### *Limitations*

This study was performed in a small sample of patients with early and mild/moderate disease, early in the pandemic, when few therapeutic interventions were available, and was restricted to those able to tolerate breathing room air. Also, recovery data were collected at only one time-point and we do not have follow-up data on all patients. Consequently, it may not be generalisable to more severe disease. Other (pre-existing) comorbidities such as anaemia may have impacted on our findings, although there was no clinical evidence of these abnormalities. The logistical limitations imposed by an acute airborne infection meant that we were unable to use more sophisticated techniques such as multiple inert gas elimination [26] or imaging tools [27].

We estimated cardiac output and  $HbP_{50}$ , required for the calculation of intrapulmonary shunt and dead space. Cardiac output was determined from its well-documented relationship to  $V'O_2$  [14, 15], which was measured;  $HbP_{50}$  was taken to be 26.8 mmHg for all participants. Sensitivity analysis for these two uncertain variables shows a minor effect over a wide range of determined intrapulmonary shunt values, with no effect on dead space [10].

#### *Conclusions*

Our study shows that in early mild/moderate COVID-19 pneumonitis, there is both increased intrapulmonary shunt and increased alveolar dead space, with marked interpatient variability and lack of correlation. These findings suggest that alveolar filling, resulting in little or no ventilation to some alveoli, and pulmonary microvascular compromise, resulting in little or no blood flow to other alveoli, are both present to varying, but separate, degrees in the early phases of mild/moderate COVID-19 pneumonitis. For essentially all patients, shunt resolved in early recovery; however, for ~30% of patients, elevated dead space persisted, at least in the early recovery phase. Characterising individual patient pulmonary

pathophysiological responses may help inform more personalised approaches to effective treatments in both the acute and recovery phases of infection with SARS-CoV-2.

**Author contributions:** The majority of the authors (P. Harbut, G.K. Prisk, C.E. Farrow, G. Hedenstierna, T.C. Amis, A. Malhotra, P.D. Wagner and K. Kairaitis) met on at least a fortnightly basis remotely. The original idea and study design were conceived in these meetings (P. Harbut, G.K. Prisk, C.E. Farrow, G. Hedenstierna, T.C. Amis, A. Malhotra, P.D. Wagner and K. Kairaitis). Ethics approval, subject identification, data collection, including clinical data, and data analysis occurred in Sweden (P. Harbut, R. Lindwall, S. Hamzei and J. Palmgren). Analysis of the raw data signals was primarily performed by G.K. Prisk, with discussion of signal analysis by P. Harbut, G.K. Prisk, C.E. Farrow, G. Hedenstierna, T.C. Amis, A. Malhotra, P.D. Wagner and K. Kairaitis, and further data analysis, including statistical analysis, in Sydney (K. Kairaitis, C.E. Farrow and T.C. Amis). All stages of the study were discussed at fortnightly meetings, including troubleshooting of protocols and quality control of the data. All authors contributed to the preparation of the manuscript and approved the final version.

**Data availability:** Individual de-identified data and the protocol used in this study will be available to investigators whose proposed use of the data has been approved by an independent review committee identified for this purpose. Data will be available for meta-analysis from 9 to 36 months of publication. After 36 months the data will be available in the Karolinska Institutet (Stockholm, Sweden) data repository but without investigator support other than the deposited data.

**Conflict of interest:** A. Malhotra has received grants from the National Institutes of Health, and consulting fees for medical education from Livanova, Equilium, Corvus and Jazz. P.D. Wagner has received consulting fees from SMS Biotechnology and Third Pole Inc., and has participated on the data safety monitoring board on Dr Levine's (UT Southwestern, Dallas, TX, USA) PPG. P. Harbut received an unconditional loan of the equipment used in this study from the Djurgården Hockey Club, Stockholm. No other author has a conflict of interest to declare.

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