TECHNICAL NOTE

Evaluation of the THRESHOLD® trainer for inspiratory muscle endurance training: comparison with the weighted plunger method

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ABSTRACT: Inspiratory muscle training (IMT) has been shown to enhance exercise performance. The weighted plunger (WP) system of inspiratory threshold loading is the most commonly used method of IMT, but is expensive and cumbersome. We have evaluated a commercially available portable spring-loaded IMT device, the THRESHOLD® trainer.

The WP and THRESHOLD® trainer devices were evaluated with their opening pressures set, in random order, at 10, 20, 30 and 40 cmH2O. Using an air-pump, pressure at the valve inlet was recorded at the point at which the valve opened, and at airflow rates of 20, 40, 60, 80 and 100 L·min⁻¹. Ten THRESHOLD® trainers were then compared using the same opening pressures and airflow rates. Finally, 10 patients with stable chronic heart failure (CHF) inspired through the WP and THRESHOLD® trainer for 4 min each. The pressure-time product (PTP) was calculated for each 4 min period, to compare the work performed on inspiring through each device.

The mean measured opening pressures for the WP set at 10, 20, 30 and 40 cmH2O, were 9.0, 19.3, 27.9 and 39.2 cmH2O, respectively, and there was little change over the range of flow tested. Corresponding values for the THRESHOLD® trainer were 7.5, 16.9, 26.2 and 39.1 cmH2O, with the pressure being closer to the set pressure as flow increased to that seen in clinical practice. The 10 different trainers tested performed very similarly to one another. Work performed (as measured by PTP) on inspiring through the WP and THRESHOLD® trainer was not significantly different.

Although less accurate than the weighted plunger, the THRESHOLD® trainer is an inexpensive device of consistent quality. In a clinical setting it would be a satisfactory option for inspiratory muscle training in most patients, but less so in patients with very low inspiratory flow rates.

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Inspiratory muscle strength and endurance have been shown to be reduced in a number of conditions, such as chronic obstructive pulmonary disease (COPD) and chronic heart failure (CHF) [1, 2]. Recently, much interest has been focused on the value of inspiratory muscle endurance training as a therapeutic option in such conditions [3]. A number of methods have been described, which can be used both to measure inspiratory muscle endurance (IME) and to train inspiratory muscles. The most commonly used method is inspiratory threshold loading, first described by Nickerson and Keens [4], in which a weighted plunger is used, requiring the subject to generate and sustain a set inspiratory pressure in order to achieve airflow. Alternative methods described include voluntary isocapnic hyperpnoea, in which subjects hyperventilate at normocapnoea to a target minute ventilation [5], and another form of threshold loading using a solenoid device [6]. In this last technique, the subject has to generate a set pressure in order to initiate airflow, but the resistance is removed once airflow begins. The last two methods both require cumbersome and expensive equipment, and can generally only be used in a laboratory setting. The THRESHOLD® trainer is, however, a commercially available portable valve device, which utilizes the principle described by Nickerson and Keens [4] and is designed for IMT. The device is small and can be used at home with ease. We have evaluated the THRESHOLD® inspiratory muscle trainer and compared it with a weighted plunger (WP) constructed in our own workshops.

Methods

In our workshops, we constructed a pressure threshold valve based on the weighted plunger principle [4]. The plunger of this valve produced a seal using a rubber ring of “V” cross-section, in an attempt to emulate...
the refinement described by Eastwood and Hillman [7] of the original plunger design. Weights are added to the plunger to increase the threshold opening pressure, the increase in pressure depending upon the size of the plunger. For our device, increments of 270 g increased the threshold opening pressure by 10 cmH₂O each. The device is illustrated in figure 1.

This valve was compared with the THRESHOLD® inspiratory muscle trainer (Healthscan Products Inc., Cedar Grove, NJ, USA), which is a spring-loaded valve, the threshold opening pressure of which can be adjusted up or down by compressing or decompressing the spring, respectively. The device has a scale of threshold opening pressure printed on its side, allowing the opening pressure to be set according to these markings. The THRESHOLD® device is illustrated in figure 2.

The behaviour of both the weighted plunger and the THRESHOLD® trainer was assessed with the opening pressure set in increments of 10 cmH₂O from 10 to 40 cmH₂O inclusive. Two hundred and seventy gram weights were added to the plunger to set the opening pressures, and the THRESHOLD® trainer opening pressure was set according to the manufacturers markings. Using an air pump (KDG 2000; KDG flowmeters, Glasgow, UK), flow through each valve was increased in increments of 20 L·min⁻¹ from 0 to 100 L·min⁻¹, at each set opening pressure. A pneumotachograph head was attached to the opening of each of the two valves, and the pressure differential across the pneumotachograph and the pressure at the valve opening were measured (SiPlan Electronics Research). For each set opening pressure, the observed opening pressure was documented. This was defined as the pressure just before airflow commenced. The pressure was also documented at airflows of 20, 40, 60, 80 and 100 L·min⁻¹. Five sets of observations were made for each device, with the opening pressures from 10 to 40 cmH₂O performed in a different random order for each set of observations.

Ten different THRESHOLD® trainers were then compared with one another. For each trainer, the opening pressure was set in increments of 10 cmH₂O from 10 to 40 cmH₂O, and the same method was used to increase airflow through the trainer from 0 to 100 L·min⁻¹ in increments of 20 L·min⁻¹. One set of observations was performed for each trainer, and the opening pressure observed was documented, together with the pressure at airflows of 20, 40, 60, 80 and 100 L·min⁻¹.

Finally, 10 patients with stable CHF inspired for 4 min both through the WP and the THRESHOLD® trainer in random order. The pressure signal was passed through an analogue-to-digital converter (SiPlan Electronics Research, Stratford-upon-Avon, UK) to an A310 Microcomputer (Acorn) sampling at 100 Hz. For each 4 min period, the total work performed by the patient was calculated as the pressure-time product (PTP). A noninvasive method of measuring PTP has been validated previously [8]. From the pressure signal, respiratory rate and duty cycle were calculated. The maximum inspiratory mouth pressure (MIP) for each patient was also measured: subjects were seated wearing a noseclip, and repeated maximal inspiratory manoeuvres were performed at functional residual capacity until two maximal values within 10% of one another were obtained. (P.K. Morgan, Chatham, Kent, UK). The highest recorded value was taken as the MIP.

Statistical comparisons were made using nonparametric tests in the FASTAT software package (SYSTAT Inc., Evanston, Illinois, USA).

Results

The THRESHOLD® valve opens at pressures several centimetres of water below the intended opening

![Diagram of the weighted plunger](image1.png)

![Diagram of the THRESHOLD® trainer](image2.png)

![Pressure recorded at the valve inlet for the weighted plunger](image3.png)
pressure, and at low flow rates the pressure remains below the set pressure. A plateau is then achieved above airflow rates of about 20 L·min⁻¹, where pressure becomes more independent of flow and more accurately reflects the set pressure. At high pressures and high flow rates, the measured opening pressure across the trainer valve exceeds the set value by up to 5 cmH₂O. The plunger behaved in a more consistent fashion, with much less deviation from the set opening pressures and very little variation in pressure with airflow. The pressure-flow characteristics of the weighted plunger and the THRESHOLD® trainer at the different set opening pressures are shown in figures 3 and 4, respectively. Table 1 shows the mean (SD) values for the 10 different THRESHOLD® trainers.

For the 10 patients studied, the mean (SD) MIP was 72 (21) cmH₂O. Figure 5 shows the PTP for each patient breathing on the WP plotted against the PTP for the THRESHOLD® valve. For each patient, there was very little difference in PTP when breathing through the WP and THRESHOLD® valve. There was also no difference in mean duty cycle or respiratory rate, which were calculated for the 10 patients on each device as follows: mean (SD) duty cycle for the WP was 0.54 (0.06) and for the THRESHOLD® valve 0.51 (0.07). The mean (SD) respiratory frequency on the WP was 15.7 (3.8) breaths·min⁻¹ and for the THRESHOLD® valve 17.2 (4.5) breaths·min⁻¹.

Table 1. – Threshold opening pressure ($P_{th}$) and pressure at different flow rates for 10 THRESHOLD® trainers

<table>
<thead>
<tr>
<th>Set pressure</th>
<th>$P_{th}$ at 20 L·min⁻¹</th>
<th>40 L·min⁻¹</th>
<th>60 L·min⁻¹</th>
<th>80 L·min⁻¹</th>
<th>100 L·min⁻¹</th>
</tr>
</thead>
<tbody>
<tr>
<td>10 cmH₂O</td>
<td>8.2 (0.8)</td>
<td>9.2 (1.0)</td>
<td>10.0 (0.6)</td>
<td>10.1 (0.7)</td>
<td>10.2 (0.6)</td>
</tr>
<tr>
<td>20 cmH₂O</td>
<td>16.9 (1.2)</td>
<td>18.6 (0.7)</td>
<td>19.7 (0.8)</td>
<td>20.3 (0.8)</td>
<td>20.5 (1.0)</td>
</tr>
<tr>
<td>30 cmH₂O</td>
<td>24.8 (1.8)</td>
<td>28.7 (1.2)</td>
<td>30.3 (1.2)</td>
<td>30.9 (1.1)</td>
<td>31.3 (1.1)</td>
</tr>
<tr>
<td>40 cmH₂O</td>
<td>37.6 (2.0)</td>
<td>39.6 (1.4)</td>
<td>40.4 (1.3)</td>
<td>41.6 (1.1)</td>
<td>42.2 (1.1)</td>
</tr>
</tbody>
</table>

Values are presented as mean, and SD in parenthesis.

Discussion

Mean inspiratory flow rates for normal subjects during inspiratory threshold loading are about 60 L·min⁻¹ [9, 10]. The fall in opening pressure below the set value at low flow rates with the THRESHOLD® trainer is, therefore, unlikely to be of relevance when training normal subjects. However, inspiratory flow rates in patients with lung disease may be lower, particularly if different breathing strategies are adopted. In patients with COPD, mean inspiratory flow rates of 25 L·min⁻¹ have been documented during inspiratory muscle endurance testing [11]. At these flow rates, the work performed by the inspiratory muscles could, in theory, be considerably less with the THRESHOLD® device than with the weighted plunger. Patients might adjust their breathing pattern to prolong inspiratory time, hence reducing inspiratory flow rates. Our data for patients with CHF suggests that the work performed with the two devices is similar.

At higher flow rates, the opening pressure is well sustained, but our experience shows that using the manufacturers scale to set the opening pressure may result in an opening pressure which differs above or below that indicated on the scale by several centimetres of water. If an accurate setting is essential, then an external pressure transducer would be required to achieve this. We have, however, shown that work performed on the two devices differs little in most cases, and any such
differences are unlikely to be significant in clinical practice.
The THRESHOLD® device is inexpensive, costing £11.50 (about 23 US$). Our weighted plunger system cost several hundred pounds to develop and build and would not be a practical option for inspiratory muscle training on a large scale. In a clinical setting, the THRESHOLD® trainer is adequate for inspiratory muscle training in most patients as it is simple to use and of a consistent quality.

References