Pulmonary haemodynamics in awake rats following treatment with endotracheal pancreatic elastase


Pulmonary emphysema induced by intratracheal elastase has been widely-used as a disease model resembling human panacinar emphysema in many aspects [1–3]. In this model, capillary segments are disconnected and folded, and diffuse loss of capillaries occurs [4]. Changes in vascular smooth muscle [5], or contractile interstitial cells [6], which may regulate hypoxic pulmonary vasoconstriction, are also suggested. Radial stress applied to the extra-alveolar vessels within the lung parenchyma should be weakened, since elastic recoil pressure surrounding the vessels is lowered [7, 8]. These findings indicate that in this animal model, pulmonary haemodynamics may be altered not only during air breathing but also during alveolar hypoxia.

However, previous studies on this model have focused mainly on the morphological and biochemical aspects and ventilatory mechanics. Very little is known about the haemodynamic features of this model. The purposes of the present study were to obtain the pulmonary haemodynamic data of the frequently-used disease model during air breathing and to evaluate the haemodynamic response to acute alveolar hypoxia. An experiment on awake rats was chosen, to eliminate the effects of anaesthesia on pulmonary circulation [9]. Haemodynamic parameters were measured via indwelling pulmonary artery and abdominal aortic catheters.

Method

Design of the study

Male Wistar rats (postnatal 9 weeks) were anaesthetized with intraperitoneal injections of pentobarbital sodium (Somnopentyl, Pitman-Moore, NJ, USA), 5 mg·100 g⁻¹ BW. To the emphysema group (Group-EL), a single endotracheal instillation of porcine pancreatic elastase (US Biochemical Co., Cleveland, USA) was administered (80 U in 0.2 ml saline·100 g⁻¹ BW) [10]. Pancreatic elastase was dissolved in saline immediately before use. To the control group (Group-C), 0.2 ml of saline·100 g⁻¹ BW was instilled. Four weeks after instillation, the haemodynamic and the histological studies were performed.

The lungs of 12 rats (n=6 for each group) were fixed intratracheally at a pressure of 20 cmH₂O (14.7 mmHg) with 2.5% glutaraldehyde in 0.1 M cacodylate buffer pH
7.4. The speed of infusion of the fixative was high, 120 ml·min⁻¹ at 20 cmH₂O (14.7 mmHg) [11]. Fifteen minutes later, the trachea was ligated and the whole lung was submerged in the same fixative. Standard methods were applied to produce haematoxylin-eosin-stained and elastic/Masson-stained tissues of the lung for histological examination. Measurements of external diameter (ED) and medial thickness (MT) of small muscular arteries displaying internal and external elastic laminae were performed with an ocular micrometer. From 12 slices of each group, sections of pulmonary arteries cut in a plane perpendicular to the long axis of each vessel were selected for morphometry. Mean values of minimal and maximal ED and of minimal and maximal MT were measured. Percentage MT was calculated as 100 × MT/ED.

Blood samples were drawn into heparinized capillaries from the pulmonary artery and aorta (0.2 ml each) for measurement of mixed venous and systemic arterial O₂ saturations (SVO₂, SAO₂). The aortic blood (0.1 ml) was also analysed for blood gases (arterial oxygen tension (Pao₂), arterial carbon dioxide tension (Paco₂) and pH). Oxygen saturation was measured by an IL-282 CO-Oximeter, and blood gas by an IL-813 blood gas analyser (Instrumentation Laboratories, Lexington, MA, USA).

Oxygen consumption (VO₂) was measured by circulating air or 10% O₂ through a CO₂ absorber and desiccant and then pumping it through the chamber. The O₂ consumed was replaced from a Krogh spirometer filled with 100% O₂ saturated with water vapour. The movement of the spirometer was recorded with a linear displacement transducer and the recorder described above. The system was run, refilling the spirometer with 100% O₂ until stable linear utilization of O₂ and thermal equilibration were achieved (about 7 min). Oxygen consumption for 5 min, while blood was being sampled, was then determined, and VO₂ was calculated, correcting the volume to standard temperature and pressure, dry (STPD) [16].

Cardiac output was calculated using the following formula and indexed per kg body weight:

\[
CO = \frac{\dot{V}O_2}{1.39 \times Hb \times (SaO_2 - SvO_2)}
\]

where Hb is haemoglobin concentration.

**Experimental sequence**

Two days after surgery, animals were placed in the Lucite chamber and the chamber was ventilated with air at 5 l·min⁻¹ for the first 5 min, and then at 2 l·min⁻¹. A 15 min acclimatization period was followed by aortic blood gas analysis in room air and the chamber was then closed. After 7 min of the thermal equilibration, measurements of oxygen consumption and haemodynamics were carried out and mixed venous and aortic blood samples were drawn. The air was then switched to 10% O₂ gas, and the chamber was ventilated at 5 l·min⁻¹ for the first 5 min, and then at 2 l·min⁻¹. Twenty two minutes were allowed to reach new hypoxic steady...
state. Measurements of \( \dot{V}_{O_2} \) and haemodynamics were again carried out. \( S_vO_2 \) and \( S_aO_2 \), and haemoglobin concentration were measured. Then, aortic blood gas analysis was performed. At the end of each experiment, the animal was anaesthetized with sodium pentobarbital and the position of the pulmonary artery catheter tip was confirmed to be in the pulmonary artery. Then, the heart was removed and placed in a 10% formalin. Seventy two hours later, the atria and the major blood vessels surrounding the heart were cut off, and the weights of right ventricle (RV) and of left ventricle plus septum (LV+S) were obtained. Then, \( RV/(LV+S) \) was calculated [17].

Haemodynamic study three weeks after instillation

Both in control and elastase-treated rats, which were not the same rats as those studied at four weeks, \( P_{pa} \) and \( P_{sa} \) were measured during air breathing three weeks after tracheal instillation. The values were compared with those obtained four weeks after instillation.

Data are presented as mean and \( \text{SEM} \). Analysis of variance (ANOVA) was used to test significance of differences between groups, and Student's paired t-test for intra-individual differences. Differences were considered significant at \( p<0.05 \).

Results

Both groups gained body weight similarly. Loss of blood due to surgery as assessed by haemoglobin concentration was also similar for both groups (table 1). Heart and respiratory rates of the two groups were not different (table 2).

The lung tissue for the elastase-treated group was characterized by diffuse and extensive dilatation and disruption of alveoli (fig. 1). There was a significant increase in percentage medial thickness of small pulmonary arteries in Group-EL (table 3).

Haemodynamics during normoxia

During normoxia, systemic artery pressure, total systemic artery resistance, cardiac index, and arterial and mixed venous blood gas data did not differ between the groups. Pulmonary artery pressure tended to be higher in Group-EL, but the difference was not statistically significant (table 2).

Ppa and PVR responses to acute hypoxia

Breathing 10% \( O_2 \) significantly lowered \( P_{sa} \) in Group-C (\( p<0.01 \)) and Group-EL (\( p<0.05 \)). \( SVR \) decreased in...
Fig. 2. – a) Response of Ppa to acute hypoxia. Sizes of the response are expressed on the right side as an absolute and as a percentage rise above the baseline. Acute hypoxic exposure significantly raised Ppa in both groups (*: p<0.01). The absolute and the percentage increase of Ppa by acute hypoxia was significantly larger in Group-EL than in Group-C (#: p<0.05). b) Response of PVR to acute hypoxia. Magnitude of the response is expressed on the right side as in a). The response of PVR to acute hypoxia tended to be larger in Group-EL, but not of statistical significance. *: p<0.01 vs air breathing. O : group-C (n=12); ■ : group-EL (n=9). Ppa: pulmonary artery pressure; PVR: pulmonary vascular resistance; Group-EL: instilled with porcine pancreatic elastase; Group-C: instilled with saline.

both groups, although the change was not statistically significant. Ten percent O₂ breathing did not cause significant alterations in cardiac index, despite consistent falls in VO₂. Ppa of Group-C increased above baseline by 25% after breathing 10% O₂ (p<0.01)(fig. 2). The rise in PVR in this group was 37% above baseline (fig. 2)(p<0.01). The increase of Ppa in Group-EL after breathing 10% O₂ was 46% above baseline, significantly higher than that for Group-C (p<0.05). Although the change of PVR in Group-EL tended to be larger than in Group-C, ANOVA did not reveal statistical difference between the two groups. However, right ventricular hypertrophy, as expressed by RV/(LV+S), occurred in Group-EL (table 1).

Table 3. – Percentage medial thickness of pulmonary arteries

<table>
<thead>
<tr>
<th>ED (µm)</th>
<th>Group-C</th>
<th>Group-EL</th>
</tr>
</thead>
<tbody>
<tr>
<td>&lt;50</td>
<td>4.4±0.3 (4)</td>
<td>7.8±0.9 (5)*</td>
</tr>
<tr>
<td>50–100</td>
<td>3.3±0.7 (6)</td>
<td>7.2±0.5 (10)**</td>
</tr>
<tr>
<td>&gt;100</td>
<td>2.0±0.6 (4)</td>
<td>6.4±1.0 (5)**</td>
</tr>
</tbody>
</table>

Data are presented as mean±SEM. Numbers in the parentheses are the number of the sections of arteries on which morphometry was made. Group-C: saline-treated group; Group-EL: elastase-treated group; ED: external diameter; *: p<0.05; **: p<0.01 vs Group-C.
Table 4. – Body weight and pulmonary and systemic arterial pressure 3 weeks after elastase instillation

<table>
<thead>
<tr>
<th>Group</th>
<th>BW g</th>
<th>Ppa mmHg</th>
<th>Psa mmHg</th>
</tr>
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<tbody>
<tr>
<td>Group-C (n=10)</td>
<td>249±4</td>
<td>17.9±0.4</td>
<td>120±2</td>
</tr>
<tr>
<td>Group-EL (n=15)</td>
<td>245±3</td>
<td>20.8±0.4*</td>
<td>119±1</td>
</tr>
</tbody>
</table>

Data are presented as mean±SEM. BW: body weight; Ppa: pulmonary artery pressure; Psa: systemic artery pressure; Group-C: saline-treated group; Group-EL: elastase-treated group; *: p<0.01 vs Group-C.

Ppa 3 weeks after elastase instillation

During air breathing Ppa of Group-EL was significantly higher than that of Group-C at this period of experiment (p<0.01) (table 4).

Discussion

This is the first description of the pulmonary haemodynamics of an emphysema model produced by intratracheal elastase. The study demonstrated that four weeks after tracheal instillation of pancreatic elastase, the change in pulmonary artery pressure when animals were exposed to 10% O₂ was significantly larger in the emphysema group than in the control group, and at this period the right ventricle was significantly more hypertrophic in the emphysema group.

In the calculation of PVR, we used the same Pcw, 3.8 mmHg, for both groups. This value is quite close to the left ventricular end-diastolic pressure of rats, 3.4 mmHg, used by Fried et al. [15]. Whilst it is possible that Pcw while breathing 10% O₂, was lowered by reduction of the blood returning to left atrium because of raised pulmonary vascular resistance [18], we assumed that the reduction of the left atrial pressure was negligible.

Different investigators have used widely varying amounts of porcine pancreatic elastase, ranging from 1.3–100 U·100g⁻¹ BW in different animal species [1, 19–22]. In earlier work, we tested dose dependency of lung pressure-volume curve and morphometry using porcine pancreatic elastase ranging from 20–100 U·100g⁻¹ BW in rats [10]. The pressure-volume curve at 100 U was more to the right and downward than at 80 U and, in addition, animal mortality shortly after instillation was higher. Mean linear intercepts of animals treated with 100 U were only slightly larger than those of animals with 80 U. From these results, we concluded that 80 U·100g⁻¹ BW is optimal for a rat emphysema model produced by a single intratracheal instillation of porcine pancreatic elastase. With 80 U, mean linear intercept was 98 μm, 1.4 times that of the control value. 72 μm [10]. This degree of widening of alveolar space corresponds to human emphysema ranging from mild to relatively severe [23]. In the emphysema model produced by elastase instillation, mean linear intercept increases between 3–6 weeks, with no other significant change, although some functional parameters continue to change over 52 weeks [24].

While breathing air, the control animals showed mean systemic artery pressure, mean pulmonary artery pressure, cardiac index, and pulmonary resistance similar to previous results obtained for awake rats [13, 15, 16, 25]. Heart rate [15, 25] and respiratory rate [26] were also similar to other reports. Mean pulmonary artery pressure of the emphysema group after 4 weeks was higher than the values of the control group, but not statistically significant. However, mean pulmonary artery pressure three weeks after instillation of elastase, was significantly higher than that of the control group during air breathing (table 4). Right ventricular hypertrophy of the emphysema model was significant, even four weeks after instillation (table 1), suggesting the existence of an experimental period of pulmonary hypertension. It seems that, in this model, pulmonary hypertension recovers earlier than medial wall thickness and right ventricular hypertrophy.

It is presently accepted that total pulmonary vascular resistance is determined by two portions of the pulmonary bed, namely, the alveolar and the extra-alveolar segments [7, 8]. To the extra-alveolar vessels within the lung parenchyma, outward radial stress is applied by the surrounding tissue, and this resists the narrowing of vascular beds. Outward force exerted on vasculature by the lung tissue during resting respiration should be weaker in Group-EL than in Group-C. Attenuation of the opposite radial force exerted on pulmonary vessels against the hypoxic pulmonary vasoconstriction is probably one of the reasons why change in pulmonary artery pressure with 10% O₂ was higher in Group-EL.

Medial walls were significantly more thickened in Group-EL. An increased medial thickness produces a vascular hyperreactivity, which does not necessitate the concomitant presence of a changed smooth muscle sensitivity-reactivity. Increase in wall/lumen ratio reduces their structurally determined lumen and tends to potentiate the luminal reductions for a given smooth muscle reduction [27]. Then, an increase in pulmonary arterial wall thickness can also explain the enhancement of hypoxic pulmonary vasoconstriction.

The third possible reason for enhanced pulmonary vascular reaction to hypoxia is an increased responsiveness of the pulmonary vascular smooth muscle. The emphysematous lung produced by an endotracheal elastase instillation showed greater contractility to KCl in vitro, in a study in which lung parenchyma included vascular smooth muscle [5].

In summary, we reported on the pulmonary haemodynamics of an emphysema model produced by a single endotracheal instillation of elastase, 80 U·100 g⁻¹ BW. With this dose and four weeks after instillation, the right ventricle was significantly more hypertrophic in treated animals than in untreated animals. The medial thickness of small pulmonary arteries of the group treated with elastase was significantly increased. Pulmonary artery pressure responded significantly more to acute hypoxia in elastase-treated animals, although the vascular reactivity was not significantly different between the groups when the pressure response was evaluated as pulmonary vascular resistance.
References


