



The effect of surgery on lung volume and conventional monitoring parameters in ventilated newborn infants

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ABSTRACT: In newborn infants, thoraco-abdominal surgery is a serious intervention with respect to gas exchange and lung mechanics. This prospective clinical study compared surgery-induced changes in functional residual capacity (FRC) and ventilation inhomogeneity (VI) indices with changes in conventional monitoring parameters.

Of 29 ventilated newborns (mean weight $2,770 \pm 864$ g at surgery), 13, nine and seven underwent thoracic, abdominal or congenital diaphragmatic hernia (CDH) surgery, respectively. The multiple breath washout (MBWO) technique using heptafluoropropane as tracer gas (Babylog® 8000; Dräger, Lübeck, Germany) was performed <6 h before surgery, 22–24 h after surgery and <6 h before extubation. Gas exchange, respiratory mechanics, FRC and VI index data were recorded.

Thoraco-abdominal surgery resulted in changes to FRC and VI indices in a procedure-specific manner; however, these changes were not reflected in conventional mechanical or ventilatory monitoring parameters. FRC decreased in non-CDH infants, while FRC increased and VI indices decreased in CDH infants. Despite improvements, the differences in FRC and VI between CDH and non-CDH infants indicated persistent impaired lung function in CHD infants.

MBWO can be advantageously used to measure the effect of surgery on the lung. While FRC and VI indices changed following surgery, conventional monitoring parameters did not.

KEYWORDS: Congenital diaphragmatic hernia, lung volume, mechanical ventilation, multiple breath washout, newborn infant, thoraco-abdominal surgery

Survival in newborn infants following corrective surgery for serious cardiac [1, 2] or abdominal wall defects [3] or for congenital diaphragmatic hernia (CDH) [4] has improved over the last decade. Nevertheless, opening the thoracic cavity and/or abdominal wall remains a significant intervention with respect to temporary alterations in gas exchange and lung volume.

In addition to ventilator monitoring, blood gas analyses and repeated radiographs are usually performed in ventilated infants to monitor clinical development. Meanwhile, commercial equipment is available to assess lung aeration by measuring functional residual capacity (FRC) and ventilation inhomogeneity (VI) indices [5–7]. This noninvasive method is based on the multiple breath washout (MBWO) measurement technique using a tracer gas [8]. However, the equipment used for simultaneously measuring airflow and molar mass of the breathing gas is generally bulky and cumbersome for routine applications in intubated

newborns or premature infants, and requires significant floor space [9]. We have recently validated a prototype of an extended neonatal ventilator for MBWO analysis in small ventilated piglets [10]. This apparatus uses a miniaturised lightweight gas sensor and heptafluoropropane (HFP) as the tracer gas.

We hypothesised that this technique can be advantageously used in a clinical setting to measure the effect of surgery on the lung. The aim of the present prospective clinical study was the use of the HFP-MBWO technique to investigate the effect of thoraco-abdominal surgery on the lung, and to compare the changes in FRC and VI indices with the changes in conventional monitoring parameters.

MATERIALS AND METHODS

Patient characteristics

This prospective clinical study was performed in the intensive care unit of the Clinic of Neonatology, Charité Universitätsmedizin Berlin (Campus

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Mitte, Berlin, Germany). 62 newborn infants born between November 2006 and June 2008 and requiring surgery were potentially eligible for the study. The inclusion criteria were anticipated surgery and written parental consent. Due to the equipment apparatus dead space volume ($V_{D,app}$) of 4.5 mL, only infants with a tidal volume (V_T) >10 mL as measured after intubation by the Babylog® (BL) 8000 (Dräger, Lübeck, Germany) were included. 33 infants were excluded due to no requirement for mechanical ventilation after surgery ($n=10$), measurements not able to be performed according to the protocol ($n=11$), a V_T <10 mL ($n=7$), or parents refusing to give consent ($n=5$).

The remaining 29 infants were divided into three groups according to the field of surgery: 13 infants had thoracic operations (congenital heart disease or oesophageal atresia), nine infants had abdominal surgery (gastroschisis, omphalocele or volvulus) and seven infants had CDH where both cavities were opened. The study was approved by the Ethical Committee of the Charité Universitätsmedizin Berlin.

Equipment for FRC measurement

FRC was measured using a modified BL 8000. Briefly, a previously described infrared HFP sensor [10] was placed between the flow sensor of the BL 8000 and the endotracheal tube (ET). The constant flow of the ventilator ranged from 8–16 L·min⁻¹ depending on the ventilatory pressure required. Using a mechanical valve, medical grade HFP (Solvay, Hannover, Germany) from a gas cylinder was fed into the inspiratory limb of the ventilatory circuit to achieve a constant HFP concentration of 0.8%. FRC was calculated according to the MBWO technique using the flow signal (flow sensor, BL 8000) and the concentration signal (HFP sensor) by a software developed by Dräger. The lung clearance index (LCI) was calculated as the number of turnovers required to lower the end tidal tracer gas concentration to 1/40th of the starting concentration. The first three moments (M_0 , M_1 , M_2) of the washout curve and moment ratios (M_1/M_0 , M_2/M_0) and the alveolar mean dilution numbers ($AMDN_1$, $AMDN_2$) were derived from calculations that commenced at the 0th breathing cycle and ended if concentrations fell below 1/40th of the initial concentration. All VI indices were calculated by purpose-built software using the data of the BL 8000, as described previously [11]. The time delay between flow sensor signal and HFP concentration was compensated for electronically. The sample rate was 125 Hz and all signals were stored.

FRC measurements were commenced manually and stopped automatically after N cycles when the amount of ventilated alveolar air ($V_T - V_D$)· N exceeded the calculated FRC by a factor of 10. In each case, the minimum number of cycles was set at $N=40$. V_D was calculated from the HFP signal by the Dräger software using the Bohr equation. An electronic two-point calibration of the HFP sensor using internal light signals and a one-point flow sensor calibration of the BL 8000 as recommended by the manufacturer was performed prior to every FRC measurement, and the equipment was also checked using a lung model before each measurement [10].

Protocol

All measurements were performed with the patient in a supine position at three defined time-points: within 6 h before

surgery, 22–24 h after surgery, and within 6 h prior to extubation.

The study protocol did not specify any ventilatory parameters, except that the mode had to be conventional or synchronised intermittent mandatory ventilation (no high frequency ventilation). Ventilation and inspiratory oxygen fraction (F_{I,O_2}) were adjusted aiming for an arterial carbon dioxide tension (P_{a,CO_2}) of between 35 and 55 Torr (4.67–7.33 kPa) and normoxia according to clinical diagnoses (e.g. cyanotic heart failure). For each FRC measurement, respiratory frequency (f_R), V_T , ET leakage and respiratory compliance (C_{resp}), which was calculated by linear regression analysis, were taken from the BL 8000.

Besides MBWO parameters (FRC, LCI, M_1/M_0 , M_2/M_0 , $AMDN_1$ and $AMDN_2$), ventilatory pressures (peak inflation pressure (PIP) and positive end-expiratory pressure (PEEP)) and blood gases were recorded. Additionally, F_{I,O_2} , arterial oxygen tension ($P_{a,O_2}/F_{I,O_2}$), P_{a,CO_2} , arterial oxygen saturation (S_{a,O_2}), blood pressure and heart rate (M1166A; Philips Medical Healthcare, Hamburg, Germany) were recorded at each of the three scheduled time-points for evaluation of circulatory parameters following surgery. Data obtained from patient charts included gestational age, birth weight, sex, multiple births, pre-natal administration of steroids, mode of delivery and Apgar scores at 1 and 5 min.

FRC measurements were performed identically at each of the three scheduled time-points. After preparation and calibration of the equipment with identical adjustment of the modified BL 8000, the ET of the infant was clamped to avoid FRC destabilisation. Within 5 s, the modified BL 8000 was connected and a stabilisation period of 15 min was allowed with continuing mechanical ventilation. Arterial blood samples for blood gases (ABL 800Flex; Radiometer Medical ApS, Bronshøj, Denmark) were then taken and FRC measurements were commenced with an HFP wash-in procedure (FRC_{wash-in}) and a consecutive washout procedure (FRC_{washout}). Such a cycle was accepted for evaluation and a mean value of FRC_{wash-in} and FRC_{washout} was calculated if the deviation between FRC_{wash-in} and FRC_{washout} was <20% and the V_T was >10 mL due to the increased $V_{D,app}$. All lung function measurements were repeated three times for each of the three situations.

Statistics

CDH is too rare a diagnosis (~1 in every 3,500 births) for a sample size calculation. A sample size of 22 was calculated only for non-CDH infants as being required to detect a FRC difference of 2 mL·kg⁻¹ after surgery, assuming a standard deviation (SD) of the FRC differences (based on a pilot study) of 3.8 mL·kg⁻¹, and an alpha error of 0.05 and a beta error of 0.1.

Patient characteristics between the patient groups were compared using Chi-squared tests and ANOVA, as appropriate. Apgar scores, age at time of surgery and duration of intubation and surgery are expressed as median and range and were compared using the Kruskal–Wallis test. All physiological parameters are presented as mean ± SD in tables and mean (95% CI) in figures. Differences between patient groups were tested using ANOVA with Student–Newman–Keul's *post hoc* test. ANOVA for repeated measurements with Dunnett's *post*

hoc test (comparison with baseline) was used to analyse parameter development. Bonferroni correction of the *p*-value for multiple within and between group comparisons was used. Statistical analysis was performed using Statgraphics Centurion software (version 15.0; Statpoint Inc., Herndon, VA, USA) and GraphPad PRISM version 4 (San Diego, CA, USA). Statistical significance was defined as a *p*-value <0.05.

RESULTS

Subjects

The three patient groups (*i.e.* thoracic, abdominal and CDH surgery) were similar in terms of pre-operative patient characteristics (table 1). Only four (13.8%) out of 29 infants had received pre-natal steroids, while two (6.9%) out of 29 had undergone surfactant treatment. While the mean bodyweights were similar for all three groups, there was a wide scatter in the time of surgery without statistically significant differences in the median after Bonferroni correction (table 2).

Ventilatory parameters, blood gases and circulatory parameters

The between-group comparison showed that before and after surgery ventilatory parameters (PIP, PEEP, *f*_R, V_T, oxygenation index and ventilatory efficacy index), blood gas parameters (P_aO₂/F_iO₂, P_aCO₂, S_aO₂) and circulatory parameters (heart rate, systolic and diastolic blood pressure) were not statistically significant different between the three patient groups. Only in CDH infants compared with the other two patient groups was *f*_R significantly higher (*p*<0.001) before surgery and V_T significantly lower (*p*<0.001) before as well as after surgery.

In all three patient groups, the within-group comparison showed no statistically significant effect of surgery on ventilatory, blood gas and circulatory parameters, respectively.

Effect of surgery on lung function

The pre-operative C_{resp} and FRC for each patient group are shown in figure 1. In CDH infants, both parameters were lower, while there were no significant differences between thoracic and abdominal surgery infants. Most pre-operative VI indices were higher in the CDH infants, whereas there were no

significant differences between the other two patient groups (fig. 2).

The development of lung function after surgery differed between patient groups (table 3). There were distinct differences in parameter progression between thoracic, abdominal and CDH surgery infants. Thoracic surgery resulted in changes in FRC, LCI and moment ratios, while C_{resp} remained nearly constant. At 24 h after thoracic surgery, FRC was lower and ventilatory VI indices, LCI and M₁/M₀ were higher (*p*<0.05). Before extubation, all pulmonary parameters returned to baseline values except for FRC, which remained elevated (*p*<0.001).

At 24 h after abdominal surgery, FRC was lower, but recovered to baseline by the time of extubation. C_{resp} also decreased after abdominal surgery, but only marginally. However, prior to extubation, C_{resp} exceeded the baseline (*p*<0.001). No significant differences were observed in the VI indices.

Parameter development differed between CDH and non-CDH infants. Besides C_{resp}, there was an improvement in all pulmonary parameters after surgery. Compared with baseline, FRC increased (*p*<0.01) and all VI indices (LCI, M₁/M₀, M₂/M₀, AMDN₁, AMDN₂) decreased (*p*<0.05).

C_{resp} and FRC were compared between patient groups prior to extubation (fig. 3). There were no significant differences in the infants following thoracic or abdominal surgery. However, despite the trend of increased C_{resp} and improvement in FRC in CDH patients, both parameters remained lower compared with the other patient groups. At extubation, there were no significant differences in VI indices between the three patient groups.

DISCUSSION

Our study has shown that HFP-MBWO is a suitable technique to measure the effect of surgery on the lung. The main finding was that FRC and VI indices measured during mechanical ventilation were more affected by surgery than conventional monitoring parameters. Furthermore, the effect on FRC and VI indices was procedure-specific.

TABLE 1 Patient characteristics at birth				
	Thoracic surgery	Abdominal surgery	Surgery of CDH	p-value
Subjects n	13	9	7	
Birthweight g	2742±1076	2076±855	2695±556	0.224
Gestational age weeks	36.6±3.5	34.4±4.3	37.9±1.6	0.134
In born [#]	9/13 (70)	7/9 (78)	5/7 (71)	0.905
Male	9/13 (69)	3/9 (33)	4/7 (54)	0.248
Caesarian section	10/13 (77)	8/9 (89)	6/7 (86)	0.847
Pre-natal steroids [†]	3/11 (27.3)	0/8 (0)	1/7 (14)	0.265
Surfactant	1/13 (7.7)	1/9 (11)	0/7 (0)	0.678
Apgar 1 min	8 (2–10)	7 (2–9)	5 (1–9)	0.078
Apgar 5 min	9 (3–10)	8 (7–9)	7 (5–8)	0.149

Data are presented as mean±SD, n/N (%) or median (range), unless otherwise indicated. CDH: congenital diaphragmatic hernia. [#]: infants were born within our hospital in the obstetric unit and were not transferred from another hospital to our unit for surgery; [†]: reduced total number due to missing data of admitted patients.

TABLE 2 Patient characteristics at surgery

	Thoracic surgery	Abdominal surgery	Surgery of CDH	p-value
Subjects n	13	9	7	
Bodyweight at time of surgery g	2992 ± 754	2581 ± 997	2680 ± 539	0.462
Age at time of surgery days	9 (1–113)	2 (1–103)	2 (2–2)	0.022
Duration of surgery min	145 (60–235)	150 (45–540)	100 (30–120)	0.091
Duration of intubation days	10.5 (3–23)	9.0 (4–25)	8.0 (6–22)	0.914
Total amount of infusion within 24 h post-surgery mL	474 ± 296	593 ± 210	741 ± 140	0.122

Data are presented as mean ± SD or median (range), unless otherwise indicated. CDH: congenital diaphragmatic hernia.

The three patient groups were similar with regard to clinical characteristics (tables 1 and 2). The wide scatter in the age of the infants undergoing thoracic and abdominal surgery reflected the diagnosis and the clinical requirements, whereas all CDH infants underwent surgery on the second post-natal day based on our standard protocol.

Before surgery, lung function measurements were similar for the infants requiring abdominal or thoracic surgery, probably because the lung was only indirectly affected. In contrast, CDH

infants with impaired pre-natal lung development [12] had lower FRC and C_{resp} and higher VI indices, indicating impaired ventilation homogeneity. Although lungs in infants requiring abdominal or thoracic surgery are thought to be probably normal, we found both groups had relatively low FRC values (16.38 ± 4.0 and 17.12 ± 3.9 mL·kg⁻¹, respectively). These observations may be explained by the findings of VON UNGERN-STERNBERG *et al.* [8] in a study of 14 anaesthetised young infants (2.76–7.5 kg; aged 0–6 months) that demonstrated that neuromuscular blockade led to a decrease in FRC from 21.3 ± 4.7 mL·kg⁻¹ to 12.2 ± 4.8 mL·kg⁻¹, which could be restored by additional PEEP of 3 cmH₂O. In our study, PEEP was applied prior to neuromuscular blockade and not changed, and FRC measurements prior to and 24 h after surgery were performed under neuromuscular blockade.

We found that the effect of surgery on lung function measurements was procedure specific. Within 24 h after surgery, FRC decreased in infants who underwent thoracic or abdominal surgery, VI indices increased in infants who underwent thoracic surgery, while FRC and VI indices improved in CDH infants (table 3). Few studies on respiratory mechanics in newborn infants measured parameters both

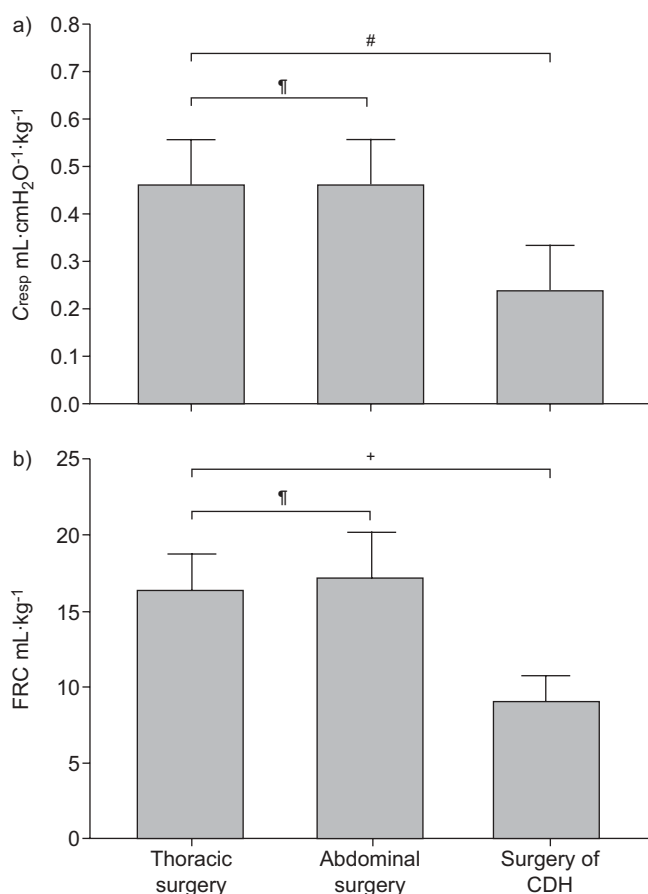


FIGURE 1. a) Respiratory compliance (C_{resp}) and b) functional residual capacity (FRC) in infants before thoracic, abdominal or congenital diaphragmatic hernia (CDH) surgery. #: $p=0.001$; ¶: nonsignificant; +: $p<0.0001$.

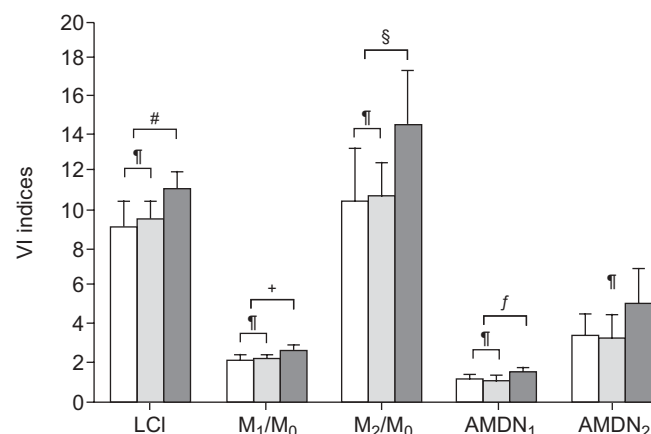


FIGURE 2. Comparison of different ventilation inhomogeneity (VI) indices in infants before thoracic (□), abdominal (■) or congenital diaphragmatic hernia (■). LCI: lung clearance index; M_1/M_0 : first-to-zeroth moment ratio; M_2/M_0 : second-to-zeroth moment ratio; AMDN₁ and AMDN₂: alveolar mean dilution numbers 1 and 2, respectively. #: $p=0.028$; ¶: nonsignificant; +: $p=0.02$; §: $p=0.033$; f: $p=0.01$.

pre- [13] and post-operatively [14, 15]. DIMITRIOU *et al.* [16] demonstrated in infants with abdominal wall defects that primary closure and surgical repositioning of the herniated viscera into the abdomen was associated with deterioration of C_{resp} . Since this observed effect was only temporary, they interpreted the decrease in C_{resp} with an increase in intra-abdominal pressure. While it appeared that the same C_{resp} trend was observed in the abdominal surgery infants in our study, the findings did not reach statistical significance.

The differences in lung function measurements between CDH and non-CDH infants were not the result of any differences in volume load, duration of operation or anaesthesia, which were similar for all three patient groups (table 2). In five patients with congenital CDH, DINGER *et al.* [17] demonstrated that FRC increased over time depending on PEEP and suctioning of the chest tube. The present FRC and C_{resp} data are similar to those reported by DINGER *et al.* [17]; however, we did not change the PEEP after surgery and chest tubes are not routinely inserted due to side-effects [4]. DINGER *et al.* [17] explained the increase in FRC in CDH infants after surgery as an over-distension of hypoplastic lungs. However, FEHRENBACH *et al.* [18] and WEIBEL [19] described lung growth following pneumonectomy in adult mice as an effect of neoalveolarisation. It remains to be seen which of these effects is responsible for the FRC gain in our

CDH infants following surgical repair and further study is necessary.

At the time of extubation, the differences in lung function measurements between CDH and non-CDH infants had reduced, yet still remained. The observed faster increase in FRC compared with C_{resp} in CDH infants agrees with a recent study by ROEHR *et al.* [20] showing that despite apparently well-inflated lungs, CDH patients had worse tidal breathing parameters and lower C_{resp} after discharge compared with non-CDH patients. Thoracic and abdominal surgery infants had similar FRCs at extubation (19.04 ± 6.0 and 18.88 ± 4.0 mL·kg⁻¹, respectively). Although all infants were successfully extubated and the neuromuscular blockade was removed, the FRC values were slightly lower than that reported by VON UNGERN-STERNBERG *et al.* [8] in intubated infants prior to anaesthetic procedures (21.3 ± 4.7 mL·kg⁻¹). However, the infants in the present study were younger and lighter than those in the study by VON UNGERN-STERNBERG *et al.* [8], and the present FRC values are consistent with those for ventilated pre-term infants [21, 22] and nonventilated full-term control infants (18.4 mL·kg⁻¹) [23].

Performing MBWO techniques in ventilated infants is difficult because the measurements are susceptible to any ET leakage [24, 25]. While this problem can be easily overcome in

TABLE 3 Development of pulmonary parameters after surgery for the three patient groups

	Before surgery	24 h after surgery	At extubation	p-value
Thoracic surgery				
C_{resp} mL·cmH ₂ O ⁻¹ ·kg ⁻¹	0.46 ± 0.16	0.42 ± 0.14	0.46 ± 0.12	0.541
FRC mL·kg ⁻¹	16.38 ± 4.0	13.89 ± 3.9*	19.04 ± 6.0*	0.001
LCI	9.25 ± 2.25	10.42 ± 1.79*	8.67 ± 2.02	0.001
M_1/M_0	2.21 ± 0.48	2.46 ± 0.42*	2.07 ± 0.5	0.003
M_2/M_0	10.61 ± 4.87	12.68 ± 4.36*	9.06 ± 4.86	0.004
AMD _{N1}	1.24 ± 0.3	1.3 ± 0.36	1.17 ± 0.21	0.341
AMD _{N2}	3.46 ± 2.07	3.85 ± 2.82	2.84 ± 1.02	0.325
Abdominal surgery				
C_{resp} mL·cmH ₂ O ⁻¹ ·kg ⁻¹	0.46 ± 0.14	0.37 ± 0.08	0.55 ± 0.16**	0.001
FRC mL·kg ⁻¹	17.12 ± 3.9	12.66 ± 4.3*	18.88 ± 4.0	0.001
LCI	9.7 ± 1.3	10.57 ± 2.31	9.07 ± 0.97	0.177
M_1/M_0	2.32 ± 0.32	2.46 ± 0.41	2.21 ± 0.23	0.287
M_2/M_0	10.87 ± 2.58	12.51 ± 4.85	9.95 ± 1.97	0.285
AMD _{N1}	1.17 ± 0.26	1.28 ± 0.49	1.21 ± 0.19	0.578
AMD _{N2}	3.34 ± 1.78	3.79 ± 3.27	3.01 ± 1.01	0.646
Surgery of CDH				
C_{resp} mL·cmH ₂ O ⁻¹ ·kg ⁻¹	0.25 ± 0.10	0.26 ± 0.09	0.29 ± 0.09	0.221
FRC mL·kg ⁻¹	8.99 ± 2.07	11.5 ± 2.92*	13.7 ± 3.61 **	0.001
LCI	11.2 ± 1.21	9.78 ± 0.77*	9.24 ± 1.08**	0.005
M_1/M_0	2.69 ± 0.36	2.34 ± 0.19*	2.20 ± 0.25**	0.006
M_2/M_0	14.6 ± 3.65	11.1 ± 1.88*	9.91 ± 2.09**	0.005
AMD _{N1}	1.57 ± 0.34	1.20 ± 0.36*	0.98 ± 0.19**	0.005
AMD _{N2}	5.20 ± 2.28	3.06 ± 1.93	2.09 ± 0.91	0.009

Data are presented as group mean ± sd, unless otherwise indicated. CDH: congenital diaphragmatic hernia; C_{resp} : respiratory compliance; FRC: functional residual capacity; LCI: lung clearance index; M_1/M_0 : first-to-zeroth moment ratio; M_2/M_0 : second-to-zeroth moment ratio; AMD_{N1} and AMD_{N2}: alveolar mean dilution numbers 1 and 2, respectively. *: p < 0.05; **: p < 0.01, when compared with measurements before surgery. Statistically significant values after Bonferroni correction are indicated in bold.

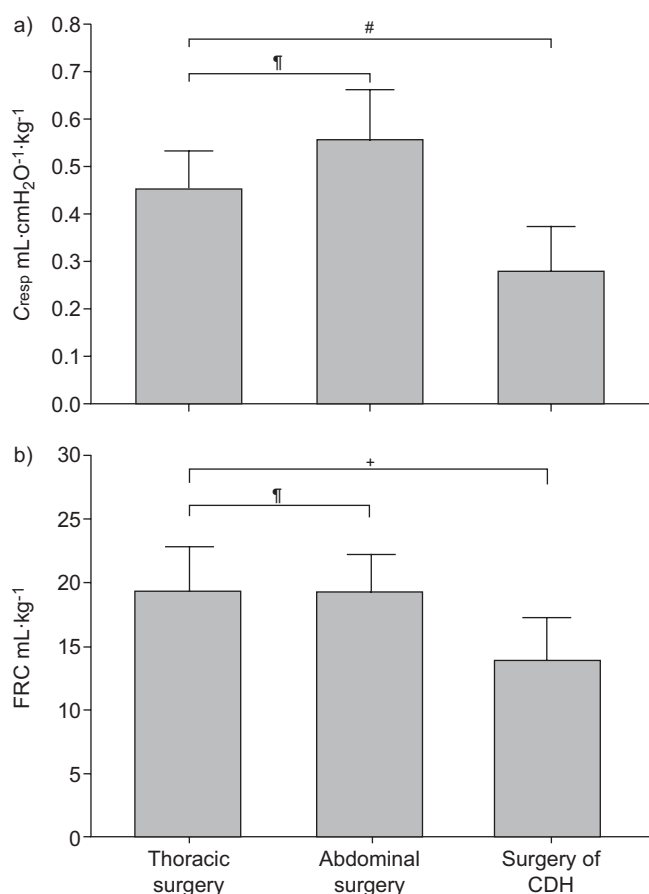


FIGURE 3. a) Respiratory compliance (C_{resp}) and b) functional residual capacity (FRC) in infants before extubation. CDH: congenital diaphragmatic hernia. #: $p=0.001$; †: nonsignificant; *: $p=0.018$.

ventilated older patients by using cuffed ETs [8], uncuffed ETs are advised in neonates both to protect airways and to avoid subglottic stenosis [26]. In our study, we could exclude a substantial effect of ET leakage on FRC measurements. During measurement we tried to avoid any ET leakage; if necessary the head position was changed. In a previous *in vitro* study, we found that the absolute value of the relative FRC error was <3% for ET leakages <20% and 6% for ET leakages <40%. In our study, the ET leakage was <20% in 95% of all infants and ET leakages of 40% were never exceeded.

Tracer gas MBWO characteristics (e.g. $V_{D,app}$, gas sensors used, properties of tracer gases and number of evaluated breathing cycles during tracer gas wash-in and washout) are also highly method dependent. Most MBWO measurements in ventilated newborns are performed using custom-made equipment and nitrogen [27], helium [28] or sulfur hexafluoride (SF_6) [7] as tracer gases. The commercial system for MBWO in ventilated patients [9] used by VON UNGERN-STERNBERG *et al.* [8] is based on ultrasound spirometry with SF_6 as the tracer gas. That equipment has a high $V_{D,app}$ and a bulky and heavy measuring head, and its use was shown to be feasible predominantly in ventilated older infants or preschool children aged from 13 months to 7 yrs [29–31]. By comparison, our HFP measuring head was designed for use in small lungs and is

smaller and lighter. While HFP and SF_6 are both inert gases, the former has a higher molecular weight (170.03 versus 146.05 $\text{g} \cdot \text{mol}^{-1}$), water solubility (0.23 versus 0.04561 $\text{g} \cdot \text{L}^{-1}$) and specific (air=1) gravity (5.9 versus 5.114) and a lower vapour pressure (4 versus 21.5 bar). Furthermore, tracer gas concentrations are lower for HFP compared to SF_6 (0.8 versus 4% [9, 32]). We recently investigated the *in vitro* accuracy of HFP-MBWO in ventilated piglets [10] and found that it allowed for reproducible measurements of FRC and VI indices, and no relevant accumulation of HFP was observed [33].

The present study found that HFP-MBWO was a valuable tool for monitoring the effect of surgery on lung function. First, a limitation of the study was the relatively low number of patients in each treatment group, which may have limited the statistical power for comparing differences in lung function and increased the risk of the type II error. The calculated sample size was only reached for non-CDH infants. Secondly, the still relatively high $V_{D,app}$ of the combined flow and HFP sensor meant that only patients with V_T values >10 mL could be investigated, which reduced the number of eligible patients. Hopefully, technical progress and increased efforts by the manufacturers will lead to new, lightweight mainstream sensors with a $V_{D,app}$ <1 mL that will enable reliable measurements even in premature infants. Thirdly, the extent to which FRC monitoring could be used to optimise ventilator settings and to realise the “open lung concept” [34] remains unknown, even in these small patients.

In conclusion, the HFP-MBWO is a suitable technique to assess the effect of thoraco-abdominal surgery on the lung. The study has shown that infants with CDH have low FRC values and impaired gas mixing before surgery, which improves, but does not normalise, thereafter. In contrast, infants receiving thoracic surgery showed a temporary decline after surgery whereas, in infants receiving abdominal surgery, little variation took place. These changes were not reflected in mechanical or ventilatory variables. A prerequisite for clinical use of HFP-MBWO is that the measuring heads be miniaturised so that measurements in premature infants are possible and that this technique is integrated into the standard monitoring of neonatal ventilators.

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STATEMENT OF INTEREST

A statement of interest for H. Proquitté, R.R. Wauer and G. Schmalisch can be found at www.erj.ersjournals.com/misc/statements.dtl

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